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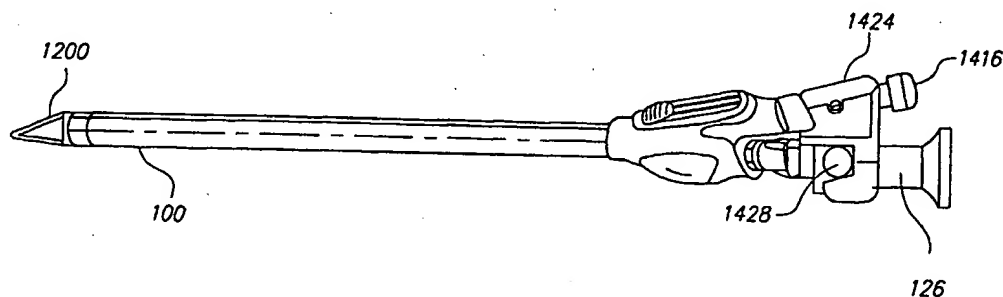
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(54) Title: COMBINED VESSEL DISSECTION AND TRANSECTION DEVICE AND METHOD



## (57) Abstract

A retractor and a surgical tool are positioned within a cannula, and a dissection cradle of the retractor is positioned at the distal end of the cannula. The retractor includes a first portion with an axis approximately parallel to the axis of the cannula and a second portion with an axis skewed relative to the axis of the cannula. The dissection cradle is located at the distal end of the second portion of the retractor, and may include two substantially parallel, spaced legs with the retractor shaped in a loop between and in a plane skewed relative to the axes of the legs, and with the loop directed away from the surgical tool. Thus, in operation, when the surgeon locates a vessel and side branch of interest, the surgeon extends the retractor to cradle the vessel in the dissection cradle. Once cradled, the retractor may be fully extended to urge the vessel away from the axis of the cannula to isolate the side branch for exposure to the surgical tool. Removable, transparent tips are selectively positioned at the distal end of the cannula for performing dissection and transection via a single cannula. Additionally, the tips are configured to align the apices of the tips with the central axis of the endoscope to maximize the visual field through the tips via the endoscope. Wing-like protrusions on an alternate tip for the cannula facilitate tissue dissection in forming a tunnel in tissue along a target vessel. Swept back forward edges on the wing-like protrusions promote easy tissue dissection using reduced force to advance the cannula and alternate tip through tissue surrounding the target vessel.

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**COMBINED VESSEL DISSECTION AND TRANSECTION  
DEVICE AND METHOD**

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10 **Field of the Invention**

This invention relates to a cannula used for vessel retraction, and more particularly to a cannula and method for performing both vessel dissection and transection.

**Cross-Reference to Related Application(s)**

The present application is a continuation-in-part application of application serial  
15 number 09/102,723 filed on June 22, 1998, and the subject matter hereof is related to the  
subject matter of application Serial Number 08/593,533 entitled "TISSUE SEPARATION  
CANNULA" filed on January 24, 1996 by Albert K. Chin, which is a continuation-in-part  
application of application Serial Number 08/502,494, entitled "TISSUE SEPARATION  
CANNULA AND METHOD," filed on July 13, 1995, which prior applications are assigned to  
20 the same assignee as the present application.

**Background of the Invention**

One important component of a surgical cannula is the tip, disposed on the distal end of  
the cannula. A properly configured tip can provide important functionality to a cannula. For  
example, the functions of vessel dissection and transection are commonly performed by two  
25 separate instruments. The device described in the pending Application Serial No. 08/907,691,  
entitled "Tissue Separation Cannula with Dissection Probe and Method," filed on August 8,  
1997, discloses a device for separating surrounding connective tissue from a vessel  
(dissection). The device described in the pending Application Serial No. 09/102,723, entitled

Vessel Isolating Retractor Cannula and Method," filed on June 22, 1998, discloses a device for retracting the vessel, ligating side branches, and transecting the branches to allow removal of the vessel. It is desirable to use a single device for performing the above functions.

5 The construction of a cannula tip also affects the visual field provided to a surgeon through an endoscope. When an endoscope is situated in a lumen of the cannula, the surgeon looks through the endoscope and through the transparent tip to view the surgical site. It is desirable to have a tip which maximizes the visual field of the endoscope.

The cannula tip may also be used to dilate a tunnel or anatomical space through tissue planes. In pending application Serial Number 09/133,136, entitled "TISSUE DISSECTOR  
10 APPARATUS AND METHOD," filed August 12, 1998, assigned to the same assignee as the present application, and which is hereby incorporated by reference, a cannula is constructed with a bulbous element near the tip of the cannula for performing tissue dilation as the cannula is advanced. Cannula tips for dilating tunnels through tissue require force in order to advance the cannula and dilate the tissue. It is desirable to have a tip which can perform tissue dilation  
15 or dissection using a minimal amount of force and causing minimal trauma.

#### Summary of the Invention

In accordance with the present invention, a tissue retractor is positioned within a cannula with a dissection cradle end of the retractor positioned at the distal end of the cannula. The retractor includes a first portion that has an axis approximately parallel to a central axis of  
20 the cannula, and a second portion that has an axis which is at an angle with respect to the central axis of the cannula. The dissection cradle is located at the distal end of the second portion of the retractor. In another embodiment, the retractor includes two legs having substantially parallel axes that selectively protrude from the distal end of the cannula. The

protruding legs support the dissection cradle formed in the shape of a loop that is positioned in a plane skewed relative to the axes of the legs, with a bottom of the loop directed away from the cannula. Thus, in operation, when the surgeon locates a vein and side branch of interest, the surgeon extends the retractor to cradle the vein in the dissection cradle. Once cradled, the  
5 retractor may be fully extended to urge the vein away from the axis of the cannula, causing the side branch to be isolated and exposed to a surgical tool. The surgical tool may then be extended from within the cannula to operate on the isolated and exposed side branch.

In another embodiment, the top of the loop of the dissection cradle is flat and thin, allowing atraumatic support of the vein, and minimizing contact between the retractor and the  
10 surgical tool. In yet a further embodiment, the retractor includes a single leg with the loop formed by the one leg of the retractor, and with a stopper coupled to the distal end of the retractor. In still another embodiment, the cannula comprises a sliding tube which encases the retractor, and in a first position is extended out to encase the second portion of the retractor, and in a second position is extended to encase only the first portion of the retractor. In  
15 response to the sliding tube being in the first position, the second and first portions of the retractor are both approximately parallel to the axis of the cannula. In response to the sliding tube being in the second position, the second portion of the retractor is skewed relative to the axis of the cannula.

In accordance with an alternate embodiment of the present invention, a removable,  
20 transparent tip is positioned at the distal end of the cannula to provide a single cannula for performing dissection and transection. When attached, the tip seals the distal end of the cannula in a fluid resistant manner. The tip is conical and ends in a sharp interior point and a slightly rounded exterior point which allows the surgeon to bluntly dissect tissue in the area of

interest under endoscopic visualization. When tissue dissection is complete, the surgeon can remove the tip from the cannula, and the surgeon is now able to use the cannula to transect side branches and vessel ends. In order to maximize the visual field provided by the endoscope, the tip is configured to allow the apex of the tip to be aligned with the central axis of the endoscope. In one embodiment, a distal end of the tip is tilted in an oblique fashion to allow the apex of the tip to align with or near to the central axis of the endoscope. In an alternate embodiment, the conical end of the tip has unequal taper angles relative to a plane of transition between the cylindrical and conical portions of the tip, thus skewing the position of the apex of the tip into alignment with or near to the central axis of the endoscope.

10 In another embodiment, wing-like protrusions are provided about the cannula near the tip to dilate tissue surrounding the vessel of interest. In one embodiment, the wing-like protrusions are diametrically aligned in a planar configuration with tapered forward edges extending rearward from near the apex of the tip. The planar configuration of the wing-like dilating protrusions near the tip substantially reduces the resistive force encountered during advancement of the cannula through tissue. The wing-like protrusions are positioned on opposite sides of the tip to dissect tissue to form a cavity that may attain a round cross-section under insufflation, thus providing the same resultant tissue dilation as provided by a solid oval dilator, but with less force required to accomplish the tissue dilation. In an alternate embodiment, the leading edges of the wing-like protrusions are curved in a parabolic configuration away from the distal end of the cannula to provide the necessary dilation.

#### Brief Description of the Drawings

Figure 1 is a perspective view of a preferred embodiment of cannula 100 showing retractor 112 in an extended position.

Figure 2a is a cut-away side view of retractor 112 and cannula 100.

Figure 2b is a top view of retractor 112.

Figure 3a is a perspective side view of cannula 100 with a saphenous vein positioned within the cradle 116.

5        Figure 3b is a perspective side view of the distal end 122 of cannula 100 in an embodiment in which an endoscope 126 and a surgical tool 120 are present and partially extended.

Figure 3c is a front view of the distal end 122 of cannula 100 in which the surgical tool 120 and the retractor 116 are partially extended, and an endoscope 126 is present.

10        Figure 4a is a cut-away top view of cannula 100.

Figure 4b is a cut-away side view of cannula 100.

Figure 5a is a cut-away view of a sliding tube embodiment of cannula 100 in a first position.

15        Figure 5b is a cut-away view of the sliding tube embodiment of Figure 5a in a second position.

Figure 6a is a cut-away view of an embodiment of cannula 100 having an angling device 140.

Figure 6b is a cut-away side view of the apparatus illustrated in Figure 6a in which the retractor 112 is extended and the angling device 140 is actuated.

20        Figure 6c is a cut-away side view of the angling device embodiment in which the angling device 140 is in a separate lumen from the retractor 112.

Figure 7a is a cut-away side view of a twistable retractor 112 in a straight position.

Figure 7b is a side view of the retractor 112 of Figure 7a.

Figure 7c is a cut-away side view of twistable retractor 112 in a crossed position.

Figure 7d is a side view of the retractor 112 of Figure 7c.

Figure 8a is a cut-away side view of the handle 104.

Figure 8b is a cut-away side view of an alternate embodiment of handle 104.

5        Figure 9a is a side view of cradle 116.

Figure 9b illustrates a first alternate embodiment of cradle 116.

Figure 9c illustrates multiple views of a second alternate embodiment of cradle 116.

Figure 9d illustrates multiple views of a third alternate embodiment of cradle 116.

Figure 9e illustrates multiple views of a fourth alternate embodiment of cradle 116.

10       Figure 9f illustrates multiple views of a fifth alternate embodiment of cradle 116.

Figure 9g illustrates multiple views of an embodiment of cradle 116 having a spur.

Figure 10a illustrates a top view of an embodiment of the cradle 116 of Figure 9c without a "C" ring.

Figure 10b illustrates a side view of the cradle 116 of Figure 10a.

15       Figure 10c illustrates a top view of the cradle 116 of Figure 9c with the "C" ring attached.

Figure 10d illustrates a side view of the cradle 116 of Figure 10c.

Figure 11a illustrates a cut-away side view of a tip 1100 in a cannula housing an endoscope 126.

20       Figure 11b illustrates a side view of the tip 1100 isolated from cannula 100.

Figure 12a illustrates a side view of an offset tip 1200 in accordance with the present invention.



Figure 12b illustrates a cut-away side view of the offset tip 1200 in a cannula 100 housing an endoscope 126.

Figure 12c illustrates a cut-away side view of an alternate embodiment of offset tip 1200.

5        Figure 13 illustrates a cut-away side view of an alternate embodiment of the offset tip 1300.

Figure 14a illustrates a perspective side view of the offset tip 1200 and mounting rod 1404.

10        Figure 14b illustrates a perspective side view of cannula 100 for housing offset tip 1200 and mounting rod 1404.

Figure 14c illustrates a perspective side view of offset tip housing 1424 at the proximal end of the cannula 100.

Figure 14d illustrates a perspective side view of cannula 100 with offset tip 1200 and offset tip housing 1424.

15        Figure 14e illustrates a perspective side view of an alternate embodiment of offset tip mount 1424.

Figure 14f illustrates a cut-away side view of the offset tip mounting 1424 of Figure 14e.

Figure 15a illustrates a side view of an alternate embodiment of offset tip 1200.

20        Figure 15b illustrates a side view of a cannula 100 modified for use with the offset tip 1200 of Figure 15a.

Figure 16 is a flow chart illustrating a method of dissecting and transecting vessels according to the present invention.

Figures 17a illustrates a top view of an embodiment of an offset tip dilator 1700 according to the present invention.

Figure 17b illustrates a side view of the embodiment of offset tip dilator 1716 of Figure 17a.

5 Figure 17c illustrates a top view of an alternate embodiment of offset tip dilator 1700.

Figure 18 is a flow chart illustrating a method of dilating tissue in accordance with the present invention.

#### Detailed Description of the Preferred Embodiments

Figure 1 illustrates a perspective view of a preferred embodiment of cannula 100 showing retractor 112 in an extended position. Cannula 100 includes an outer housing 102 of bioinert material such as polymed UD that may be approximately 12" to 18" in length. The proximal end of the cannula 100 is disposed in handle 104 that includes a button 106 which is coupled to retractor 112 for controlling the translational movement of retractor 112, as described in more detail below.

15 The distal end of the cannula houses a retractor 112, and optionally an endoscope 126 and a surgical tool 120, described below. Figure 2a illustrates the retractor 112 in more detail. In one embodiment, retractor 112 is formed of resilient wire which has a smooth bend intermediate to a first portion 110 and a second portion 114 of the retractor. The retractor 112 is described as having two portions for ease of description, although the retractor 112 may be  
20 formed as an integrated structure. However, retractor 112 may also be manufactured from two separate portions 110, 114 that are coupled together. The first portion 110 of the retractor 112 is positioned within the cannula 100 with the axis 111 of the first portion 110 approximately parallel to the axis 101 of the cannula 100. The second portion 114 is positioned to bend away

from the central axis 101 of the cannula. The angle 117 of displacement between the axis 115 of the second portion and the central axis 101 of cannula 100 may be any angle from zero to 180 degrees. The second portion 114 includes a dissection cradle 116 at the distal end of the second portion 114. The retractor 112 may be formed of bioinert material such as stainless steel, or a polymer such as nylon or polyetherimide, or other appropriately strong and resilient plastic. In one embodiment, the retractor 112 includes a coating for lubrication, insulation, and low visual glare using, for example, parylene or nylon 11.

Figure 2b illustrates the retractor 112 formed with two legs. The legs 141, 142 of the retractor 112 at the distal end form the dissection cradle 116 in a loop or "U" shape, as shown in Figure 2a. The top portion 144 of the U-shaped bend is preferably flattened to provide additional surface area for atraumatically supporting a vein 118 or vessel of interest. The side arches 128 of the dissection cradle 116 are used for skeletonizing or dissecting the vein from the surrounding tissues, as well as acting as walls to keep the vessel captured within the arch. The several embodiments of dissection cradle 116 are described in more detail below.

Figure 3a illustrates a perspective view of the cannula 100 in accordance with the present invention with the retractor fully extended, holding a saphenous vein 118, and also illustrates an external surgical tool 120 disposed adjacent the cannula 100 for performing a surgical operation, for example, severing a tributary or side branch of the vein 118. The vein is positioned within the side arches 128 of the cradle 116. The dissection cradle 116 may be used to cradle a vein, vessel, tissue or organ of interest, and surgical tool 120 may be any surgical tool suitable for performing a surgical procedure near the dissection cradle 116.

Figure 3b illustrates a perspective view of cannula 100 in an embodiment in which the surgical tool 120 is positioned within the cannula 100, and an endoscope 126 is present. In

this embodiment, cradle 116 preferably overlays the endoscope 126 with sufficient clearance to facilitate relative movements thereof. However, the endoscope may also be located adjacent the surgical tool 120. In one embodiment, endoscope 126 is positioned with cannula 100 to allow a clear field of view upon extension of the retractor 112. Surgical tool 120 is illustrated  
5 as cauterizing scissors, used to sever a tributary or side branch of a saphenous vein 118. In this embodiment, surgical tool 120 is maximally displaced from the cradle 116 at the cannula end 122. More specifically, as shown in Figure 3c, the "U"-shaped loop 129 of the cradle 116 is closest to the surgical tool 120. This ensures that a vein 118 or other tissue of interest is retracted away from the surgical tool 120 to facilitate manipulating the surgical tool 120  
10 relative to the side branch or other tissue.

Figure 4a is a cut-away top view of cannula 100. The retractor 112 is slidably positioned within minor lumens 113 along the length of the cannula 100 within close tolerances in order to position the retractor 112 stably within the cannula 100. For example, in one embodiment retractor legs 141, 142 are approximately .045 inches in diameter and the  
15 lumens 113 encasing the legs 141, 142 are approximately .080 inches in diameter, as friction between the legs of the retractor 112 and the lumens 113 holds the retractor stably within the cannula. This configuration restricts rotational movement of the retractor to provide more stable retraction as compared with conventional retractors. The legs 141, 142 of the retractor 112 are formed of flexible, resilient material and are retained within the lumen 113 in  
20 substantially straight or flat orientation, but may return to a material bend or curve, as illustrated in Figure 5a, as the retractor 112 is extended from the distal end of the cannula 100.

The leg 141 of the retractor 112 passes through a sliding gas or fluid seal 130 at the proximal end of the lumen 113. The leg 141 of the retractor 112 passes out of the cannula 100

and into handle 104 for attachment to a slider button 106 for facilitating translational movement of the retractor 112 from the proximal or handle end of the cannula 100. However, other types of control devices such as knobs, grips, finger pads, and the like may be linked in conventional ways to the retractor 112 in order to manually control the translational movement of retractor 112. In one configuration, the proximal end of leg 141 is bent relative to the axis of the cannula, and the button 106 is attached to the bent position of the leg 141 to facilitate moving the button 106 and the retractor 112 translationally under manual control. The button 106 preferably includes lateral grooves to prevent finger or thumb slippage during sliding manipulation of the retractor 112.

10        Thus, in the operation of a preferred embodiment, a user actuates the slider button 106 to extend retractor 112 out of the lumen 113 at the distal end of the cannula 100. In one embodiment, the resilient retractor 112 is formed in a smooth bend, as shown in Figure 2a, and gradually deflects away from the central axis 101 of the cannula 100 as the retractor is extended. Upon encountering the target vessel or tissue of interest, the vessel is restrained in the cradle 116, and a lateral resilient force is exerted on the target vessel in a direction away from the cannula. The vessel is thus pushed away from the axis of the cannula 100, isolating it from surrounding tissue or adjacent vessels such as tributaries or side branches. As a tributary is thus isolated, a surgical tool 120 such as cauterizing scissors may be safely employed to operate on the tributary without harming the saphenous vein 118. When retracted into the 15 cannula 100, the retractor 112 is again resiliently straightened or flattened.

20        In an alternate embodiment as illustrated in Figures 5a and 5b, a sliding tube 132 is added to provide operational versatility to cannula 100. In a first position, the sliding tube 132 is retracted and the retractor 112 protrudes from the distal end at an angle with respect to the

central axis 101 of the cannula 100. In a second position, the sliding tube 132 is extended out, temporarily straightening the retractor 112. As illustrated in Figure 5a, a sliding tube 132, in a first position encases the retractor 112 up to the point at which the retractor 112 curves away from the central axis 101 of the cannula thus allowing the retractor 112 to displace and isolate  
5 a target vessel. The proximal end of the sliding tube 132 is linked to button 107 for translationally moving retractor 112 as well as actuating the sliding tube 132. In one embodiment, as illustrated in Figure 5a, the sliding tube 132 is in a first position with the button 107 in an upright position. A spring 134 is coupled between a support structure 135 and the proximal end 137 of the sliding tube 132. In the first position of sliding tube 132, the  
10 spring 134 is extended fully and exerts little or no force on the sliding tube 132. Of course, sliding tube 132 may be manually manipulated without linkage to a button 107.

To extend the sliding tube 100, button 107 is pushed down. As illustrated in Figure 5b, the button 107 has a cam surface 136 which pushes on the proximal end 137 of the sliding tube 132 as the button 107 is pressed. The sliding tube 132 is pushed forward, overcoming the  
15 resilient force of spring 134, to encase the retractor 112 and decrease angle 117 between the distal end of the retractor 112 and the central axis 101 of the cannula 100. Upon releasing the button 107, the spring force urges the proximal end 137 of the sliding tube 132 back toward the first position against button 107. The sliding tube 132 is formed of material having sufficient strength to force the retractor 112 to straighten out the angle 117, and the retractor  
20 112 is formed of resilient material having a sufficient flexibility to straighten out the angle 117 in response to a tube 132 being slid over the retractor 112, but having sufficient rigidity to cradle and dissect a target vessel. Resiliency of the retractor 112 ensures return to the downwardly-curved shape after being released from tube 132. Thus, in accordance with this

embodiment, a user may employ the curved retractor for certain applications and employ the straightened form for other applications. A manual actuator may be configured in other ways than button 107 to extend the sliding tube 132 in response, for example, to being pulled up instead of pushed down.

5        Another embodiment employs a retractor 112 which has a naturally straight shape. As illustrated in Figures 6a and 6b, an angling device 140 is disposed between the distal end of the retractor 112 and the proximal end of the cannula. The angling device 140 may be positioned within the same lumens 113 as the retractor 112 and preferably may comprise two wires coupled to points below the cradle 116 of the retractor 112 substantially in parallel  
10    positions on each of the legs 141, 142.

      Upon extending the retractor 112 using button 106, the angling device 140 is extended with the retractor 112. The angling device 140 is coupled to a handle 145 at the proximal end of the cannula 100 to facilitate establishing an angle in the retractor 112 by pulling with a backward force on the angling device 140. As illustrated in Figure 6b, after the retractor 112  
15    is extended, the angling device 140 is actuated and a bend is created in the retractor 112 as the backward force exerted on the distal end of the retractor is exerted against the relatively fixed position of the retractor legs 141, 142 disposed within the lumens 113. As shown in Figure 6c, the angling device 140 may also be located in a separate lumen 202 from the retractor 112 with part of the angling device 140 positioned outside of the cannula 100 when the retractor 112 is  
20    in the retracted position.

      Figure 7a illustrates another embodiment of cannula 100 in which the retractor 112 is pre-formed with one leg 141 of the retractor 112 bent at an angle at its proximal end skewed to the axis of the distal end of the other leg 142. The bent portion of the leg 141 may be linked to

a sliding knob 147 for convenient manual manipulation of this embodiment of the invention. Upon sliding the knob 147, the leg 142 coupled to knob 147 is twisted rotationally. The two legs 141, 142 of retractor 112 are coupled together via cradle 116. The axis of the second portion of the retractor 112 in the first position is at a first angle 117 to the axis of the cannula 100, as shown in Figure 7b. As knob 147 is moved, leg 141 is rotated and crosses under leg 142, as shown in Figure 7c. This causes cradle 116 to flip 180 degrees and bends the retractor 112 at a second angle 119, as shown in Figure 7d. Thus, if a vessel is disposed on one side of cradle 116 or cannula 100 while the retractor 112 is in the first position, then upon rotating the knob 147, the vessel is transported to the other side of the cannula 100. This allows the user to isolate the vessel by simply actuating knob 147.

Figure 8a illustrates a cut-away side view of button 106 on the handle 104 of cannula 100, with an endoscope 126 positioned within cannula 100. As mentioned above, button 106 is coupled to one leg 141 of the proximal end of retractor 112. Sliding the button 106 in groove 146 translationally moves the retractor 112. Groove 146 is preferably minimally wider than the shaft of button 106 to minimize excessive horizontal movement of button 106 while still allowing smooth translational movement of button 106. As illustrated in Figure 8b, the button 106 may include locking or ratcheting teeth 152 to give tactile feedback of its location, and to positively retain the button and the associated leg 141 in an extended or retracted position. Several mating teeth 148 are located underneath groove 146, and a spring member 150 is attached to button 106 to exert pressure against the base of groove 146, to engage mating teeth 148, 152. When a force is applied on the top of button 106, the interlocking sets of teeth are disengaged and button 106 can move freely. Upon achieving the desired extension



or retraction of the leg 141, button 106 is released and is retained place by the engaged teeth 148, 152.

Figure 9a illustrates a top view of cradle 116 in an embodiment in which the cradle 116 is formed by two legs 141, 142 of retractor 112. The distal end of the legs form "U"-shaped side guides. The top 144 of the distal portion of the "U" is preferably flattened. This provides atraumatic support for the target vessel retained within cradle 116. Additionally, by minimizing the thickness of distal portion 144, contact with other devices in close proximity with retractor 112 is minimized.

The cradle 116 may have other effective shapes, for example, as illustrated in Figure 9b in which a "C" ring element is attached to legs of the cradle 116. The "C" ring may have a small hole 200 in one side with an axis approximately parallel to the axis of the retractor 112. This hole 200 is used to hold suture or other ligating materials, and may also be used as a knot pusher. As shown in Figures 10a and 10b, in an alternate embodiment of the embodiment of Figure 9b, the retractor 112 is formed and flattened and a "C"-shaped ring is coupled to the retractor 112 by, for example, gluing or molding the "C" ring to the distal end of the retractor 112, as shown in Figure 10c and 10d.

Referring back to Figures 9c, 9d, and 9e, the side guides of the cradle may include a loop 129 in a "V" shape, an arced "U" shape, or a semi-circular shape. In one embodiment, as illustrated in Figure 9f, the retractor 112 has only one leg 141, and the cradle 116 is formed by the leg 141. A stopper 160 is coupled to the end of the leg 141 to serve as a guide to retain the target vessel, and add a blunt surface to the end of the wire, for example, for pushing and probing tissue. Figure 9g illustrates a retractor 112 having a spur 204 formed in one or both legs 141, 142 for allowing the retractor 112 to be used for dissection. Sinusoidal, half-

sinusoidal, and other geometric configurations may be used equally effectively as the shape of loop 129 in accordance with the present invention.

Figure 11a illustrates a tip 1100 for use with a multi-lumen cannula 100 housing an endoscope 126. The tapered tip 1100 may be removed from, and reattached to the distal end of a cannula 100, as desired. Upon attachment, the tip 1100 seals the distal end of a cannula 100 in a fluid-tight manner. The tip 1100 is configured to provide dissection of the tissue surrounding the vessel of interest, and has a distal radius of approximately 0.045" to reduce the hazard of penetrating the vessel of interest. The inner surface of the tip 1100 tapers to a sharp interior point and a slightly rounded exterior point and the tip 1100 has a uniform wall thickness. The tip 1100 preferably has taper angles of approximately 15° which provides a maximal, undistorted, visual field through an endoscope 126. The tip 1100 tapers outward to a maximal diameter of about 12 3/4 mm at its shoulder to cover the cannula 100 body which also has a diameter of about 12 3/4 mm. All of these features allow the tip 1100 to effectively dissect tissue. The tip 1100 of Figure 11a has a central axis 1150 aligned with the central axis 1108 of the cannula 100. The visual field provided by the endoscope 126, although satisfactory for surgical procedures, is not complete because the endoscope 126 is in a lumen that is offset from the central axis 1108 of the cannula 100. The endoscope 126 is offset because of the space required inside the cannula 100 for housing retractors and other instruments in adjacent lumens. Figure 11b illustrates this tip 1100 detached from the cannula 100.

Figure 12a illustrates an offset tip 1200 for a cannula 100 in accordance with the present invention. The offset tip 1200 is a transparent, tapered tip as described above for use in endoscopic dissection of a vessel. However, in this embodiment the axis 1250 of the tip

1200 is skewed relative to the central axis 1108 of the cannula 100. The axis 1250 of the tip 1200 is skewed approximately  $8^\circ$ , an angle that is chosen to align the apex 1232 of the tip 1200 with a central axis 1112 of the endoscope 126, as shown in more detail in Figure 12b.

Figure 12b illustrates the offset tip 1200 housed in cannula 100 in more detail. The cannula 100 houses a 5 mm endoscope 126 having a central axis 1112 eccentric to the central axis 1108 of the cannula 100. In order to bring the distal end or apex 1232 of the axis of the tapered tip 1200 into the center of the visual field along the central axis 1112 of the endoscope 126, the tapered tip 1200 is tilted or inclined by approximately  $8^\circ$  toward the lumen housing the endoscope 126. This allows the apex 1232 of the tip 1200 to approximately intersect with the central axis 1112 of the endoscope 126. As illustrated in Figure 12b, the tip 1200 is inclined toward the central axis 1112 of the endoscope 126 without altering the taper angles 1236 and 1240 of the side walls. This is accomplished by forming a transition 1228 between the proximal or cylindrical portion 1204 of the tip 1200 and the distal or conical portion of the cannula body 1208 of the tip 1200 substantially along a plane 1230 that is skewed from normal to the central axis 1108 of the cannula 100. The distal portion 1208 of the tip 1200 retains its conical shape and equal taper angles 1228, 1236 between the side walls and the transition plane. The slight extension of the cannula body at the transition plane provides sufficient incline to allow the apex 1232 of the tip 1200 to intersect the central axis 1112 of the endoscope 126. The tip 1200 may be formed of separate conical and cylindrical parts that are attached together, or the tip 1200 may be formed as an integrated structure in the shape thus described.

Alternatively, as shown in Figure 12c, the tip 1200 is inclined at a lesser angle, for example, 5 degrees, toward the axis 1112 of the endoscope 126, positioning the axis 1250 of

the distal end 1232 of the tip 1200 intermediate between the central axis 1108 of the cannula 100 and the axis 1112 of the endoscope 126. Positioning the axis 1250 of the tip 1200 to this intermediate point allows the retention of steep conical angles in the tip 1200 which allow for easier advancement of the cannula 100 while using a minimal amount of force. The  
5 intermediate positioning also provides a more complete visual field as seen through endoscope 126.

An alternate embodiment of an offset tip 1200 is shown in Figure 13 in which the taper angles 1320, 1324 of the side walls are selected to form the apex 1328 of the tip 1200 aligned with the central axis 1112 of the endoscope 126. As illustrated, the lower region 1316 of the  
10 cylindrical part 1304 extends beyond the upper region 1312 of the cylindrical part at a plane of transition between cylindrical and tapered regions of the tip. However, in this embodiment, the taper angles 1320, 1324 are not equal and the thirty degree angled conical configuration of the tapered part 1308 is not maintained. Rather, the lower taper angle 1324 is increased to an obtuse angle and the upper taper angle 1320 is a reduced acute angle relative to the plane of  
15 transition between the cylindrical and tapered portions of the tip. In this configuration of the conical portion 1308, the apex 1328 of the tip 1200 aligns with the central axis 1112 of the endoscope 126. Thus, in accordance with either embodiment, a tip 1200 is provided which allows a maximal visual field to be viewed by the surgeon via the endoscope 126 that is eccentric the central axis 1108 of the cannula 100, but that is aligned with or near to the apex  
20 1232 of the tip 1200.

Figure 14a illustrates a perspective side view of the offset tip 1200 and mounting rod 1404. The tip 1200 is attached to the cannula 100 via the long rod 1404 which extends through an eccentric lumen of the cannula 100, as shown in Figure 14b, and the apex of the tip

1200 is tilted away from the rod 1404 and towards the endoscopic lumen (not shown). The elongated rod 1404 may be attached to the tip 1200, or may be constructed as an integral part of the tip 1200. The elongated rod 1404 preferably is secured in housing 1424, shown in Figure 14c, via threads 1408 on the proximal end of rod 1404 and mating threads within nut or knob 1416. The rod 1404 and housing 1424 abut against the proximal end of the cannula handle 1412, as illustrated in the perspective side view of the assembled device shown in Figure 14d. Referring back to Figures 14a-c, the housing 1424 includes a slot 1420 configured to slip over the light cable outlet 1428 on the endoscope 126 as assembled within the cannula 100. The housing 1424 preferably contains a rotating nut 1416 which accepts the threaded proximal end 1408 of the rod 1404. When tightened onto the rod 1404, as shown in Figure 14d, the housing 1424 prevents the cannula 100 from rotating about the endoscope 126 by holding the endoscope 126 fixed with respect to the handle 1412. This allows the operator to maintain the correct orientation of the endoscope 126 on the vessel. If the endoscope 126 is allowed to rotate freely, the image may turn sideways or upside down without the operator realizing it, and injury may occur to the vessel if the cannula 100 is advanced in the wrong direction.

In one embodiment, as shown in Figures 14e and 14f, the elongated rod 1404 slips into the housing 1424 via a groove 1450 near its proximal end, and passes through the main hole 1454 in the housing 1424. The groove 1450 allows for the housing 1424 to cover the proximal end of the mounting rod 1404 without completely clearing the most proximal tip of the mounting rod 1404. This allows more room for attaching the housing 1424 which lies between the elongated rod 1404 and additional optical components. The rod 1404 may contain an elastic section, or the rod 1404 may be somewhat elastic along its entire length to facilitate

stretching the rod 1404 and pulling it into position in the slot 1454 on the housing 1424, while locking the tip 1200 in place. The elastic force also facilitates sealing the tip 1200 against the distal face of the cannula body.

Figures 15a and 15b illustrates an alternate embodiment of offset tip 1200 and cannula 100. In this embodiment, offset tip 1200 is formed with an elongated case 1500 which slides over the cannula body 100 and locks to the proximal end of cannula 100. In this embodiment, proximal end of cannula 100 is threaded and allows a threaded proximal section of elongated case 1500 to mate securely to the cannula 100.

In a surgical procedure using the tissue-dissecting cannula of the present invention, the surgeon first incises 1600 the skin overlying a vessel of interest to expose the vessel as an initial step of the procedure illustrated in the flow chart of Figure 16. A scissor tool is inserted 1602 into the incision to create a path to the vessel by dissecting the overlying tissue. Next, the tip 1200 of the cannula 100 is inserted 1604 into the incision to bluntly dissect tissue to form an initial tunnel along the vessel from the incision. The incision is then sealed 1608 using a blunt tip trocar and a tunnel is insufflated 1612. The cannula is advanced 1616 along the vessel to dissect tissue adjacent the vessel under endoscopic visualization through the transparent tip. The offset tip 1200 with the apex thereof in alignment with the endoscope 126 provides a full visual field for the surgeon as the cannula 100 is advanced. The conical end of the tip 1200 dissects the tissue as the cannula 100 is advanced along the vessel. The surgeon dissects both on the anterior and posterior sides of the vessel to create a full 360 degree tunnel around the vessel. Once a selected surgical site is reached, the cannula 100 is removed 1620 from the incision seal and the tip 1200 is removed 1624 from the cannula 100. In one embodiment, as described above, the tip 1200 is removed by unscrewing the threaded portion

1408 of the rod 1404 from the rotating nut 1416. The tip housing 1424 itself is also removed in this embodiment. Insufflation is maintained and the cannula 100 without tip 1200 is inserted 1628 into the seal into the tunnel adjacent the vessel. Transecting devices are then inserted 1630 into the cannula 100. Without tip 1200 disposed over the distal end, the cannula  
5 100 can now be used for transecting 1632 side branches and the ends of the vessel of interest using endoscopic instruments that are selectively installed and removed within instrument lumens in the cannula body 100. After these procedures are completed, the vessel may be removed 1636.

Figure 17a illustrates another embodiment of an offset tip dilator 1700. In this  
10 embodiment of the present invention, the tip 1700 also includes wing-like protrusions for enlarging or dilating a peri-vascular cavity in the course of separating a vessel from adjacent connective tissue. For example, after tissue dissection with an offset tip 1200 to form a tunnel or working cavity adjacent a target vessel by dissecting along the anterior and posterior sides of the vessel, the cannula 100 is removed from the distal end of the body, the offset tip 1200 is  
15 detached, and a second tip 1700 is attached to the distal end of the cannula body 100. In one embodiment, the second tip 1700 includes a transparent tapered tip with planar wing-like protrusions or extensions disposed proximal to the distal end 1720 of the tip 1700. The wing-like protrusions 1702, 1704 each include a swept back leading edge. As shown in Figure 17b, the tip 1200 is tilted away from the mounting rod 1404 to align with the central axis of an  
20 endoscopic lumen (not shown). The wing-like protrusions 1702, 1704 may also include curved distal and proximal edges, for example, in a parabolic configuration as shown in Figure 17c, providing a smoother withdrawal of the cannula 100 from the insufflated tunnel. The tip 1700 attaches to the cannula body 100 in the same manner as previously described with

reference to the offset tip 1200, with an elongated rod 1404 extending through a lumen of the cannula 100 and locking at the proximal end of the handle 1412. The cannula 100 may thus be advanced through tissue under full-field endoscopic visualization through the tapered tip 1720 with the wing-like protrusions 1702, 1704 extending substantially diametrically to facilitate  
5 tunnel dilation.

The wing-like protrusions 1702, 1704 of the tip 1700 are arranged in substantially planar geometry in contrast to the solid bulbous, oval element described above. The planar configuration of the wing-like protrusions 1702, 1704 substantially reduce the frontal profile of the dilator required to penetrate tissue, and thus reduces the resistive force encountered  
10 during advancement of the cannula 100 through tissue. Although the tissue-dilating force is exerted on tissue surrounding the cavity in a bilateral, substantially planar orientation by the outer edges of the wing-like protrusions 1702, 1704 that dissect tissue forming the cavity walls, the dilated cavity may retain a round cross-section for example, within an insufflated cavity, in the same manner as if tissue dilation was performed using a solid oval dilator that  
15 applies dilating force circumferentially.

Figure 18 illustrates a method of dilating tissue in accordance with one method embodiment of the present invention. The skin is incised 1800 overlying the vessel of interest, and the scissor tool is inserted into the incision to create a path to the vessel by dissecting the overlying tissue. The incision is then bluntly dissected 1804 using the offset tip 1200 to expose  
20 the vessel surface. The incision is sealed 1808 and a tunnel is insufflated 1812. The cannula 100 is advanced 1816 along the vessel under endoscopic visualization through the transparent tip 1200. After sufficient length of tunnel is formed adjacent the vessel, the cannula 100 is removed 1820 and the incision seal is removed or slid backwards to the proximal end of the



cannula 100. The offset tip 1200 is then replaced 1824 with the dilating tip 1700. The seal is reinserted and the incision is sealed 1826. The cannula 100 is advanced 1828 and the cavity is further dilated responsive to the advancement of the planar wing-like protrusions 1702, 1704 through tissue forming the tunnel walls. The cannula 100 is removed 1832 a second time, and  
5 the incision seal is again removed or slid backwards to the proximal end of the cannula 100. The dilating tip is removed 1836 and the incision is sealed 1837. Transection devices are loaded 1838 through instrument lumens within the cannula body 100 into the cannula 100 and the cannula 100 is then inserted 1839 back into the incision. Without any tip covering the distal end of the cannula 100, the vessel side branches and ends are transected 1840 using  
10 endoscopic instruments, and the vessel is then removed 1844 from the dilated tunnel.

CLAIMS

What is claimed is:

1. A surgical apparatus for use with an elongated cannula having an endoscopic lumen for supporting an endoscope, the endoscopic lumen having a central axis eccentric to a central axis  
5 of the cannula, the surgical apparatus comprising:

a transparent tip positioned at a distal end of the cannula, having tapered walls  
converging toward a distal end, the distal end having an axis near the  
central axis of the endoscopic lumen, for providing visualization  
through the transparent tip via an endoscope within the endoscopic  
10 lumen.

2. The surgical apparatus of claim 1 further comprising:

a proximal portion, attached to a distal end of the cannula; and  
a distal portion, attached to a distal end of the proximal portion to form a  
transition plane between the proximal and distal portions skewed  
15 normal from the central axis of the cannula, for positioning a distal end  
of the distal portion near the central axis of the endoscopic lumen.

3. The surgical apparatus of claim 2, wherein the proximal portion further comprises:

a cylindrical tube, having an upper region and a lower region, in which a distal  
end of the upper region extends beyond a distal edge of the lower  
20 region; and the distal portion further comprises:

a conical end, having an upper and lower region, in which a proximal end of the lower region extends proximally beyond a proximal edge of the upper region.

4. The surgical apparatus of claim 3 wherein taper angles formed relative to a plane of transition between the cylindrical tube and the conical end are equal.
5. The surgical apparatus of claim 1 wherein the tip further comprises:
  - a cylindrical proximal portion; and
  - a conical end portion, wherein the conical end portion has unequal taper angles relative to a plane of transition between the cylindrical and conical portions of the tip, for aligning the distal end of the conical portion with the central axis of the endoscopic lumen.
6. The surgical apparatus of claim 1, wherein the tip further comprises:
  - a conical portion, positioned at a distal end of the tip; and
  - a mounting rod, attached to a proximal end of the conical portion, having a locking section disposed at a proximal end of the mounting rod.
7. The surgical apparatus of claim 6, wherein the cannula comprises:
  - a mating lock, disposed at a proximal end of the cannula, for mating with the locking section of the mounting rod and preventing rotation of an endoscope relative to movement of the cannula.
8. The apparatus of claim 1 wherein the distal end of the transparent tip is positioned to align the axis of the distal end with the central axis of the endoscopic lumen.

9. An apparatus for dilating tissue, comprising:
- an elongated cannula, having a distal and proximal ends; and
  - a tapered tip, attached to the distal end of the elongated cannula, comprising:
    - a pair of protrusions extending laterally from the tip, each protrusion
    - 5 positioned on opposite sides of the tip.
10. The apparatus of claim 9, wherein the pair of protrusions are in a planar configuration and are tapered towards the distal end of the cannula.
11. The apparatus of claim 10, wherein the pair of protrusions are in a planar configuration and curved in a parabolic configuration.
- 10 12. The apparatus of claim 9, wherein the pair of protrusions have distal ends disposed near the distal end of the tip.
13. A method of dissecting and transecting vessels using a cannula having a selectively displaceable tip disposed on the distal end of the cannula, the tip having an axis aligned with a central axis of an endoscopic lumen which is eccentric to a central axis of the cannula,
- 15 comprising the steps of:
- incising skin to expose an area near a target vessel;
  - bluntly dissecting the incision to expose the target vessel;
  - sealing the incision;
  - insufflating a tunnel along the target vessel; and

advancing the cannula through tissue along the target vessel under endoscopic visualization through the offset tip to form a tunnel in tissue adjacent the target vessel.

14. The method of claim 13 further comprising the steps of:

- 5           removing the cannula from the tunnel;
- removing the offset tip from the distal end of the cannula;
- inserting the cannula into the tunnel through the incision; and
- transecting side branches and vessel ends under endoscopic visualization through use of endoscopic instruments in cannula.

10   15. The method of claim 14 performed using a transparent dilating tip having a pair of protrusions bilaterally extending therefrom, the method further comprising the steps of:

- substituting the dilating tip for the offset tip;
- advancing the cannula under endoscopic visualization through the dilating tip along the insufflated tunnel to dissect tissue surrounding the tunnel in
- 15           response to advancement of the cannula and dilating tip therethrough;
- removing the cannula and dilating tip from the tunnel; and
- removing the dilating tip.

16. A method of dissecting and transecting vessels using a cannula having a selectively displaceable transparent tip disposed on the distal end of the cannula, comprising the steps of:

- 20           incising skin to expose an area near a target vessel;
- bluntly dissecting the incision to expose the target vessel;
- sealing the incision;

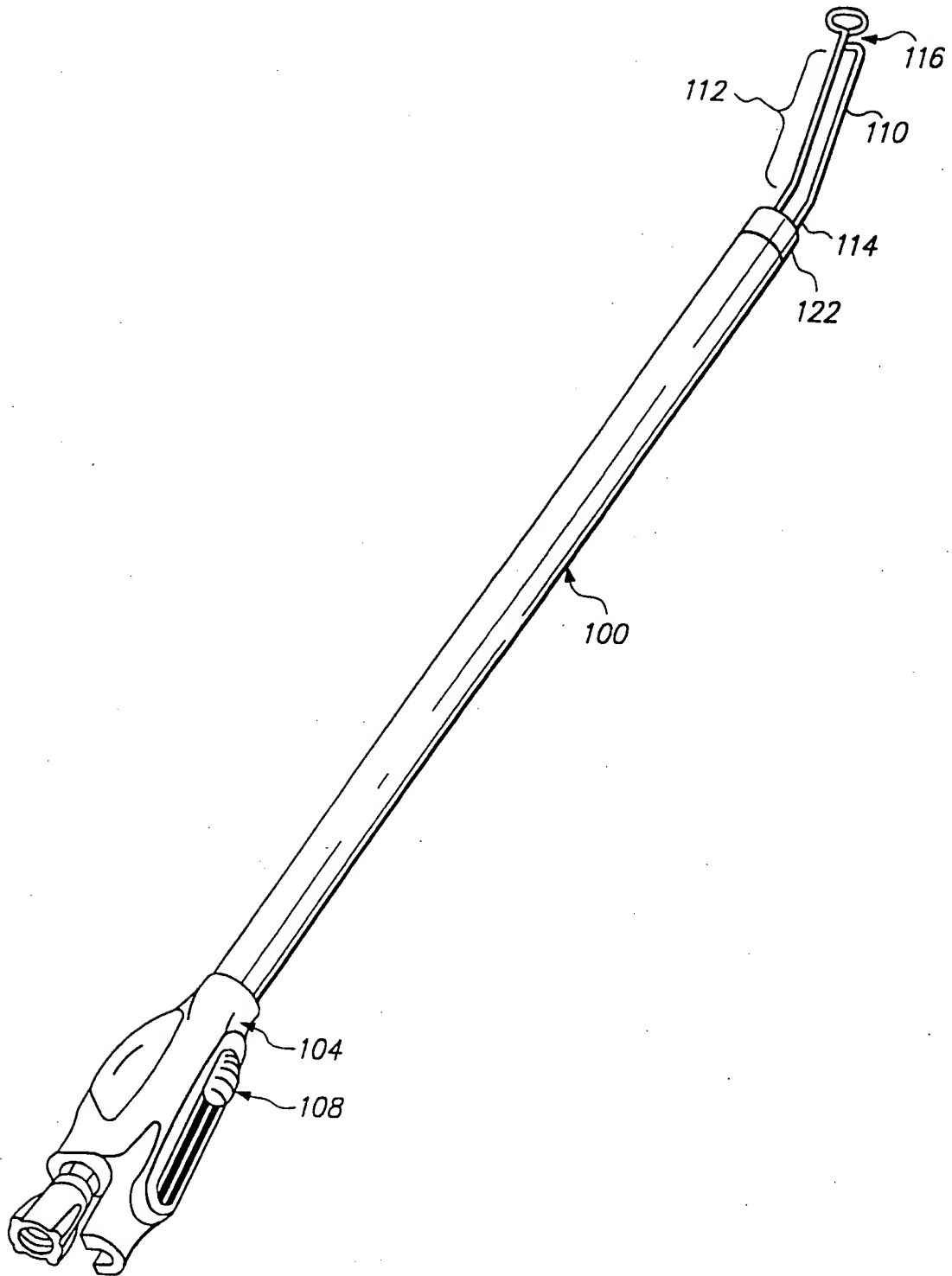
insufflating a tunnel along the target vessel; and  
advancing the cannula through tissue along the target vessel under endoscopic  
visualization through the transparent tip to form a tunnel in tissue  
adjacent the target vessel.

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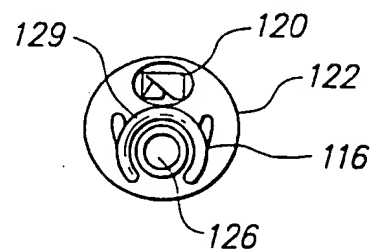
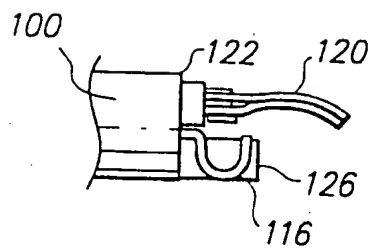
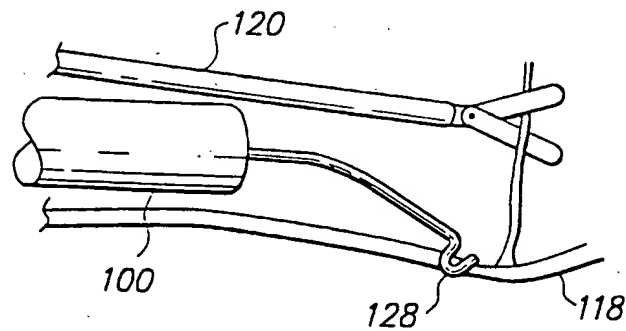
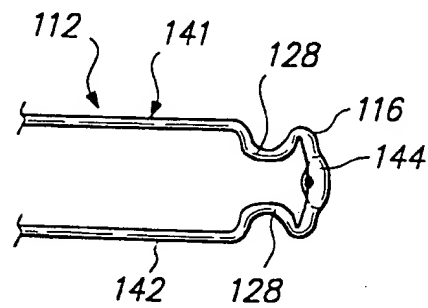
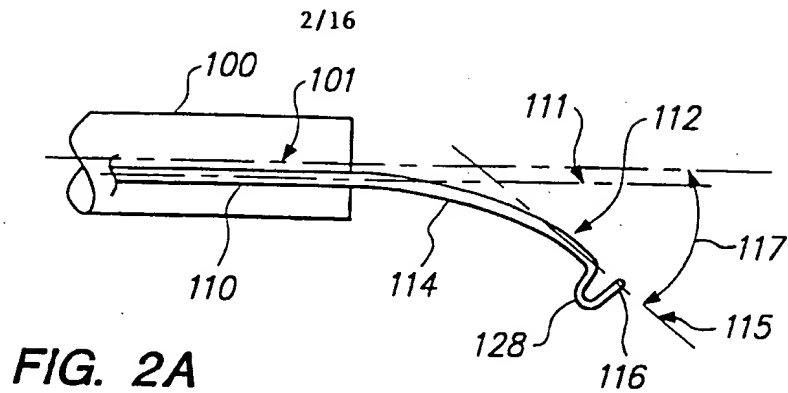
removing the cannula from the tunnel;  
removing the tip from the distal end of the cannula;  
inserting the cannula into the tunnel through the incision; and  
transecting side branches and vessel ends under endoscopic visualization  
through use of endoscopic instruments in cannula.

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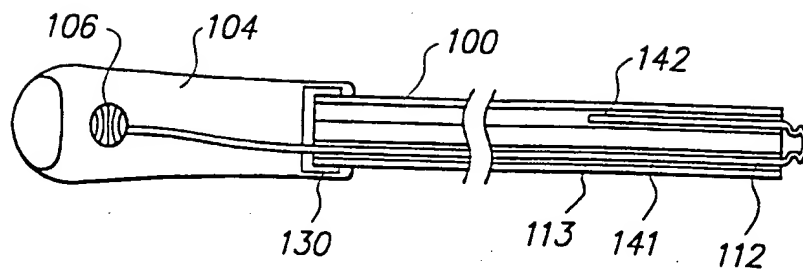


**FIG. 1**

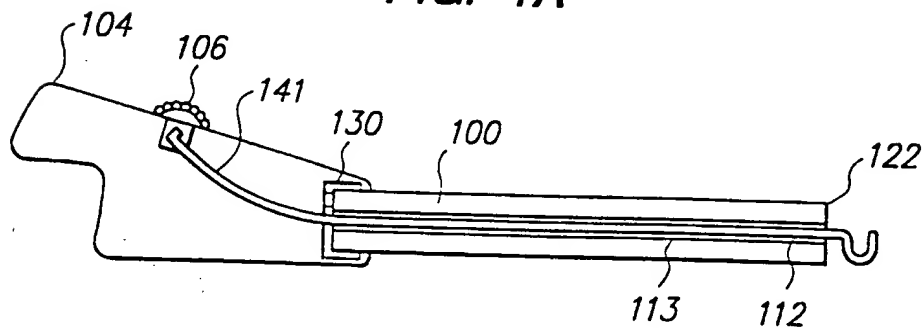




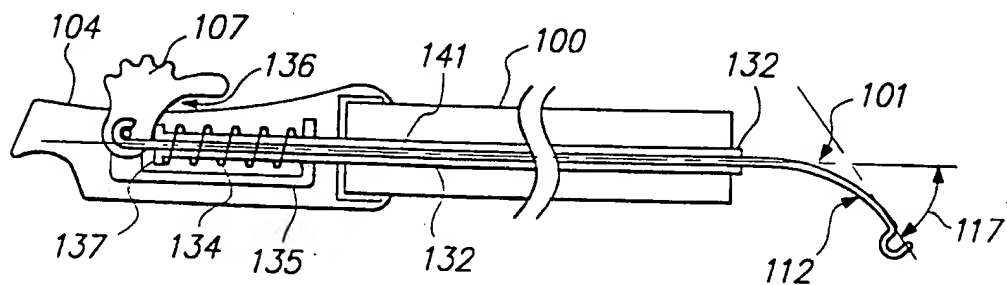
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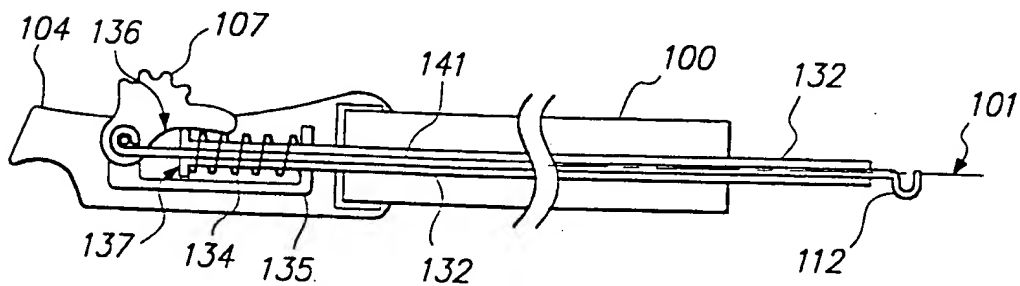
**FIG. 4A**



**FIG. 4B**



**FIG. 5A**



**FIG. 5B**

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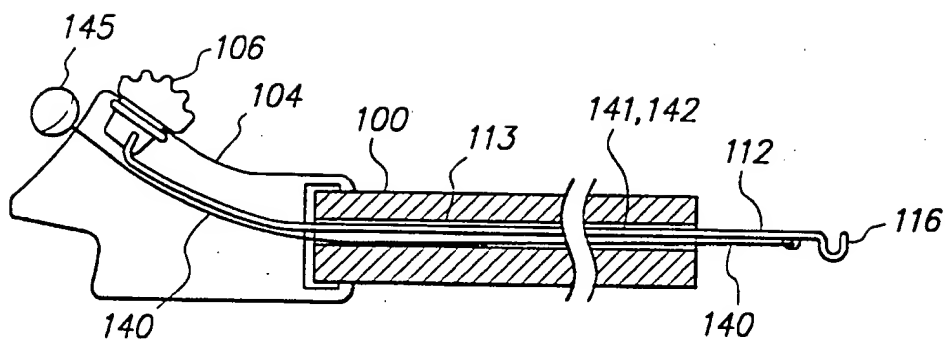


FIG. 6A

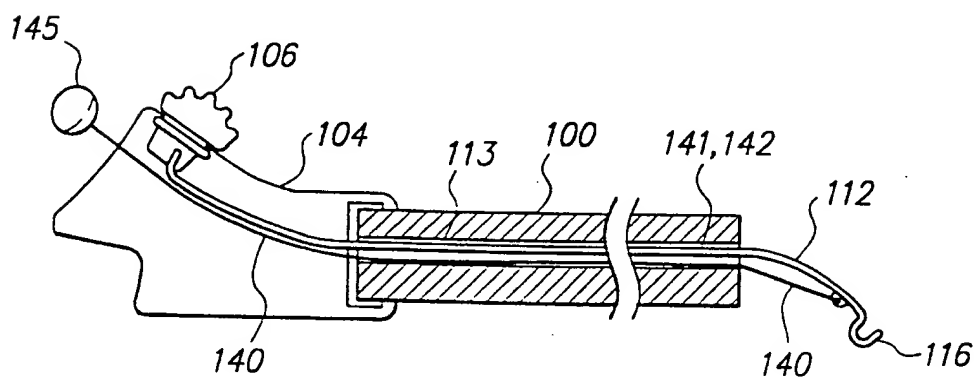


FIG. 6B

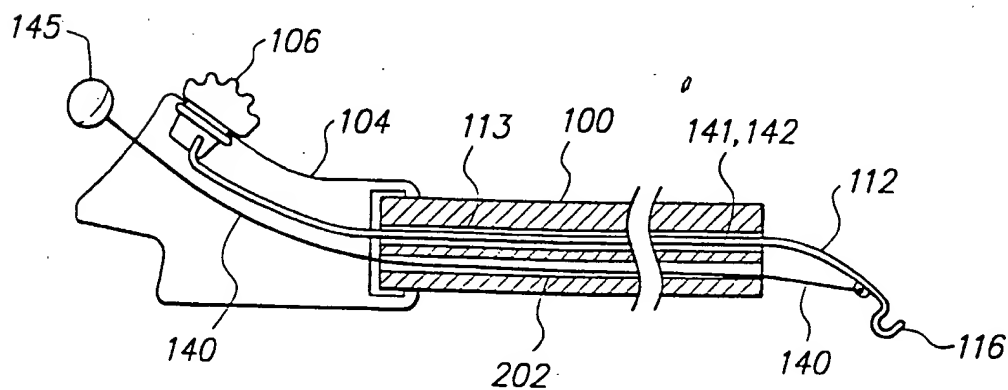
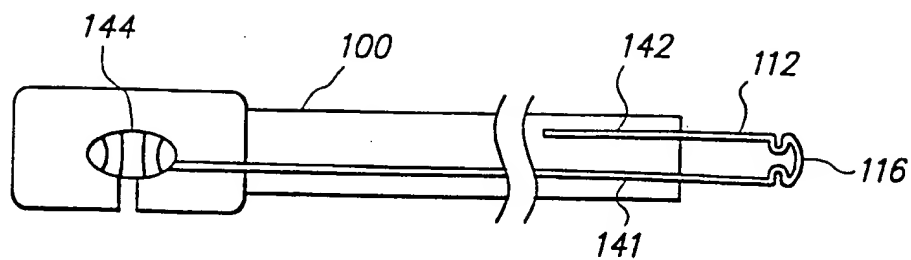
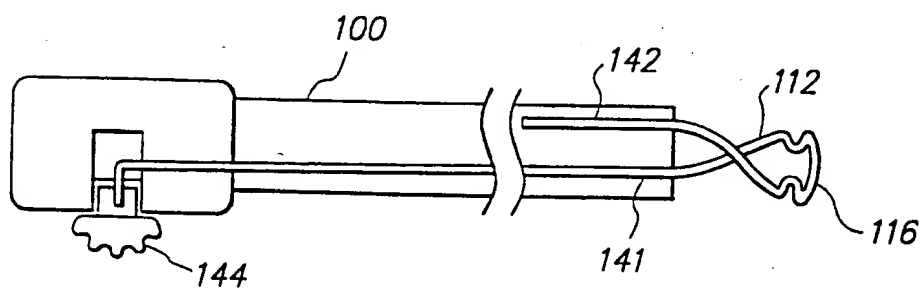


FIG. 6C

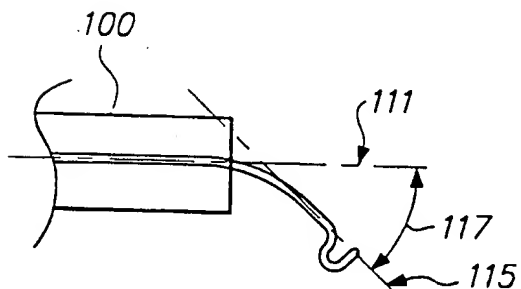
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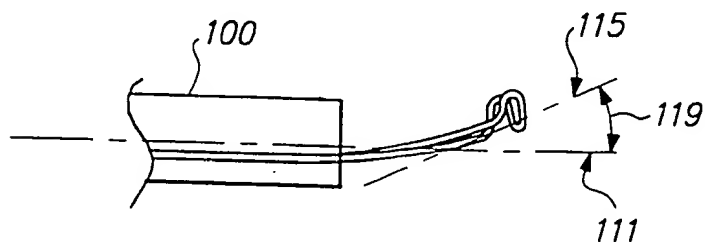
**FIG. 7A**



**FIG. 7C**

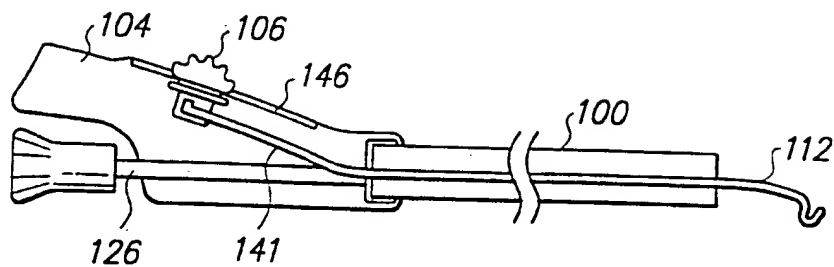


**FIG. 7B**

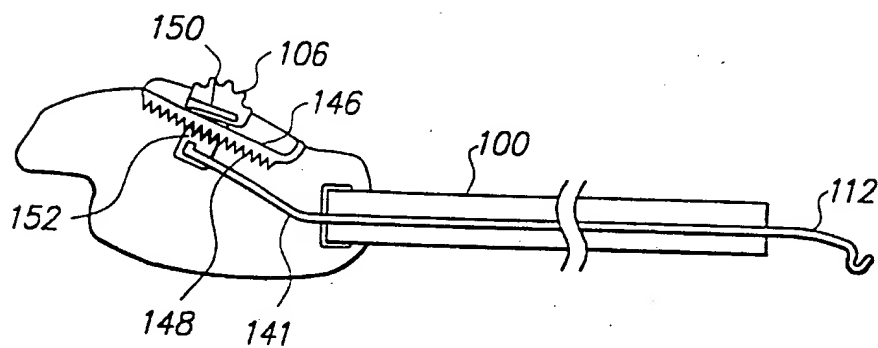


**FIG. 7D**

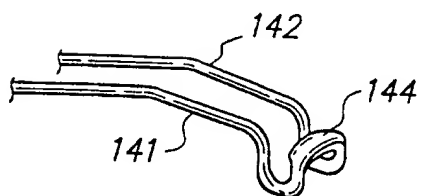
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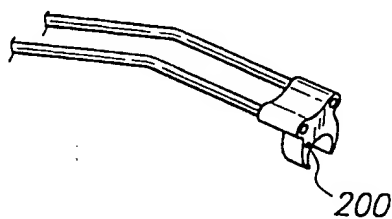
**FIG. 8A**



**FIG. 8B**

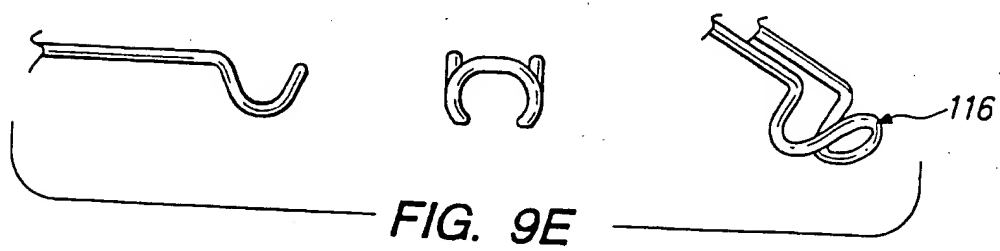
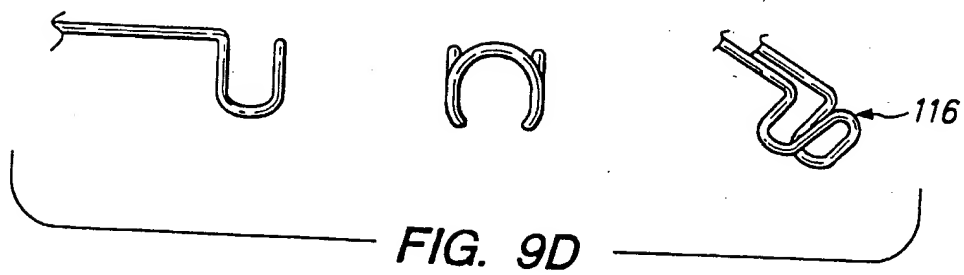
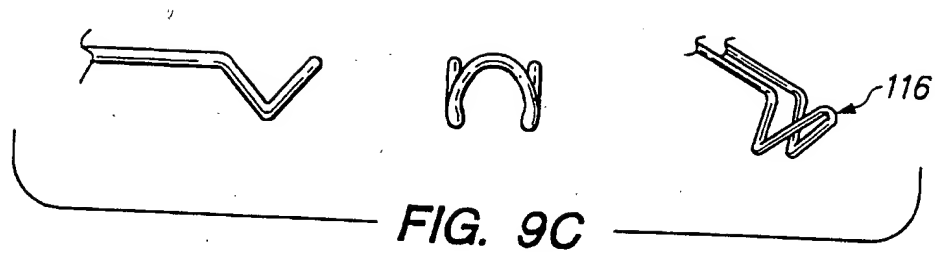


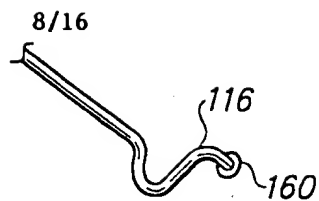
**FIG. 9A**



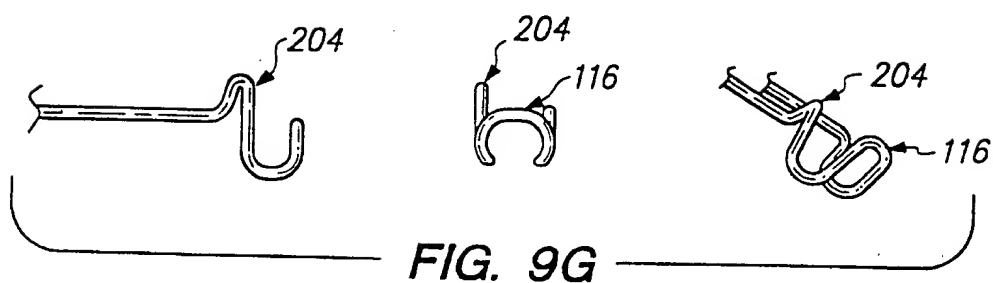
**FIG. 9B**

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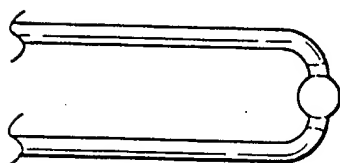




**FIG. 9F**



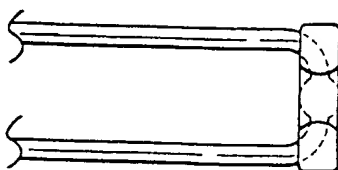
**FIG. 9G**



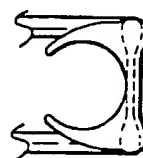
**FIG. 10A**



**FIG. 10B**

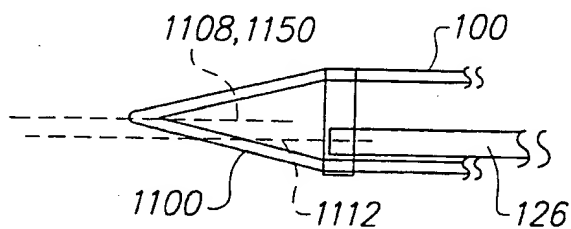


**FIG. 10C**

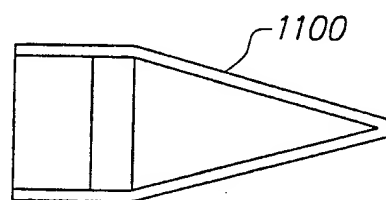


**FIG. 10D**

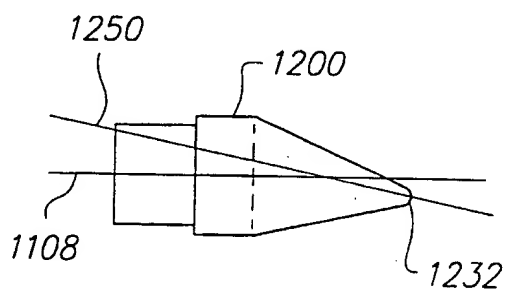
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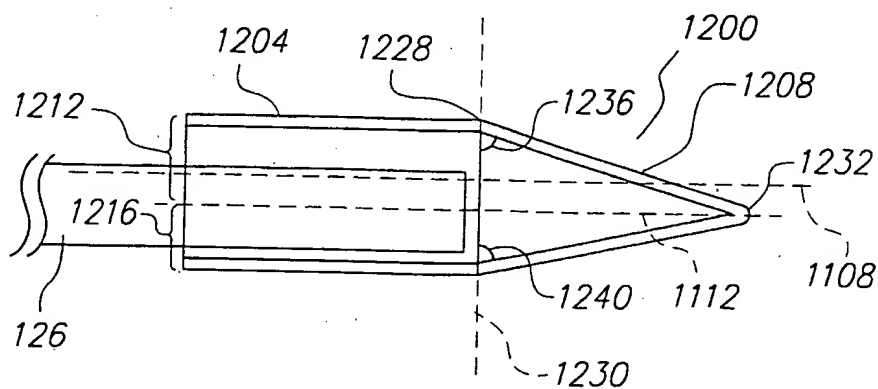
**FIG. 11A**



**FIG. 11B**



**FIG. 12A**



**FIG. 12B**

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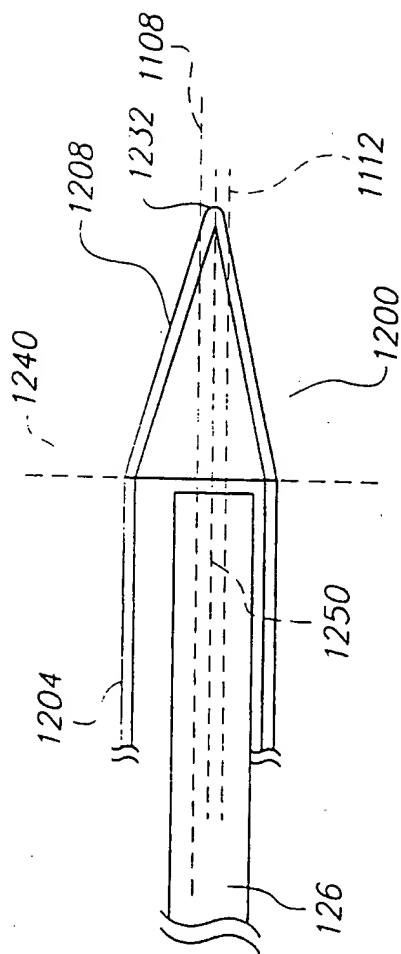


FIG. 12C

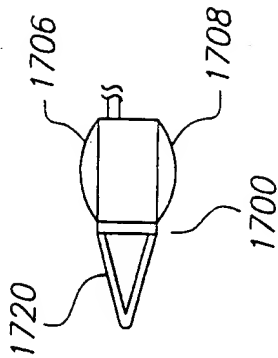


FIG. 17C

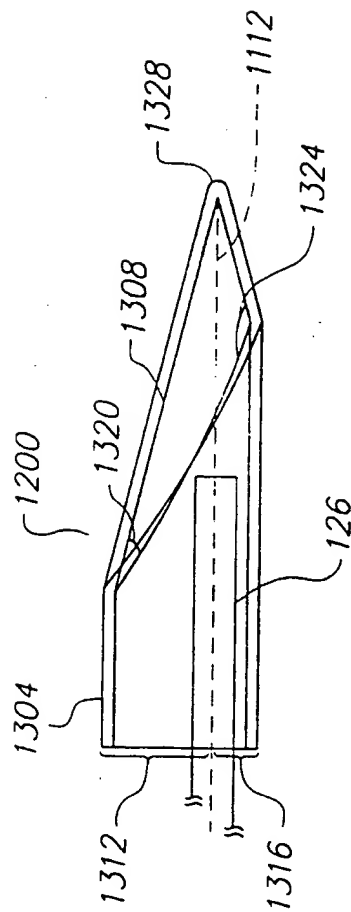
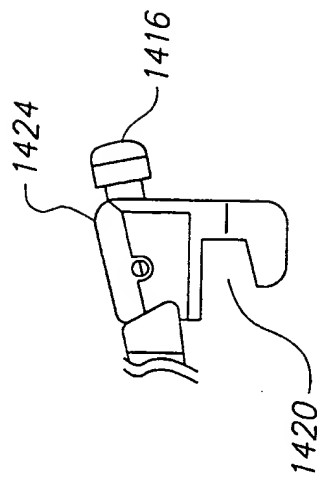
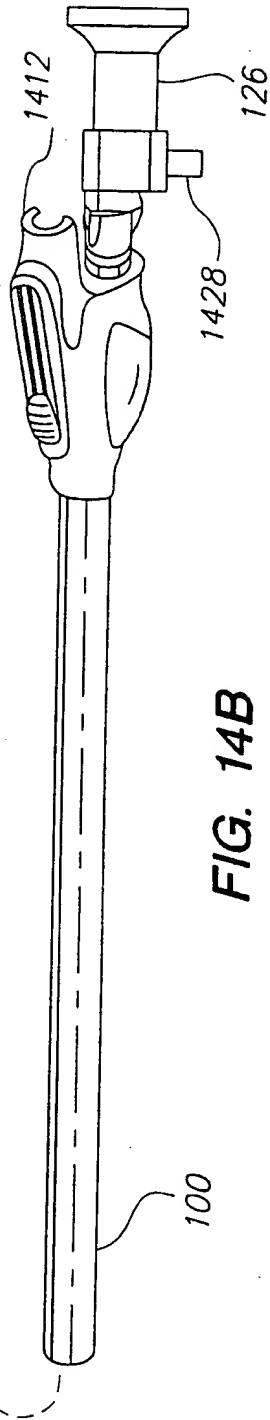
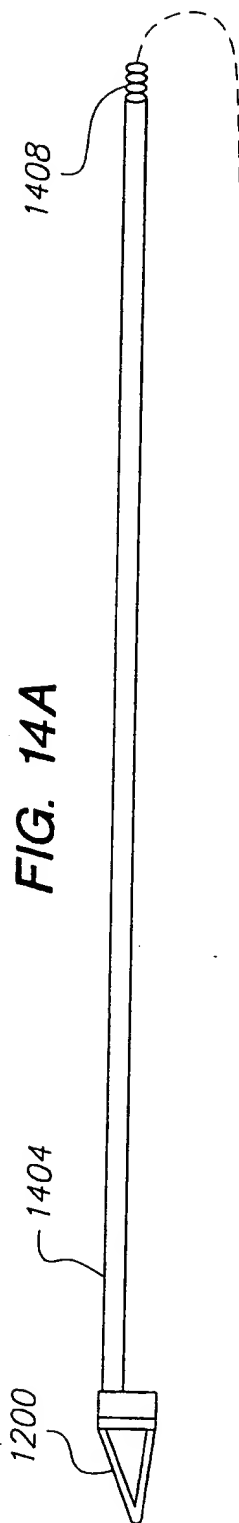


FIG. 13



11/16



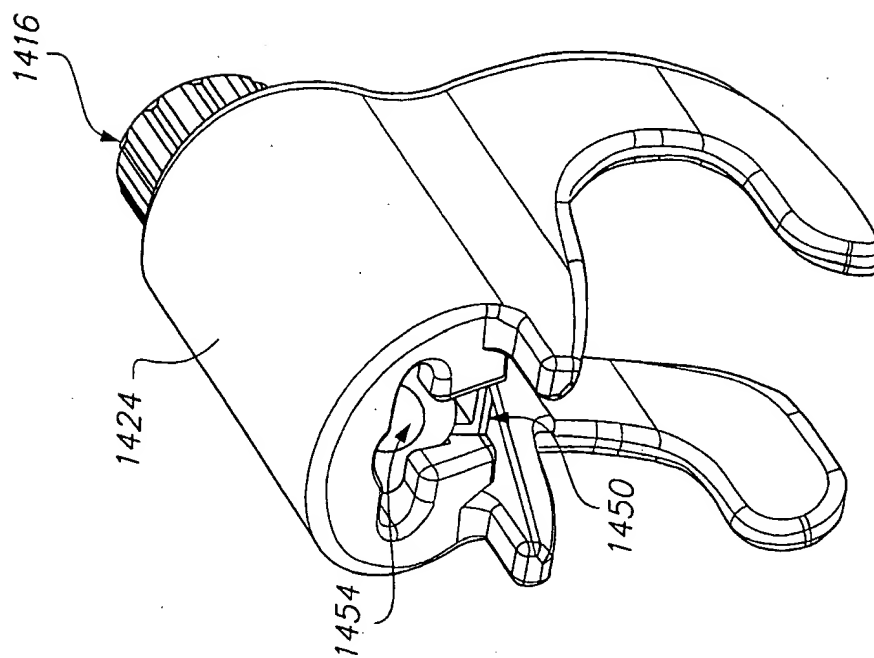


FIG. 14E

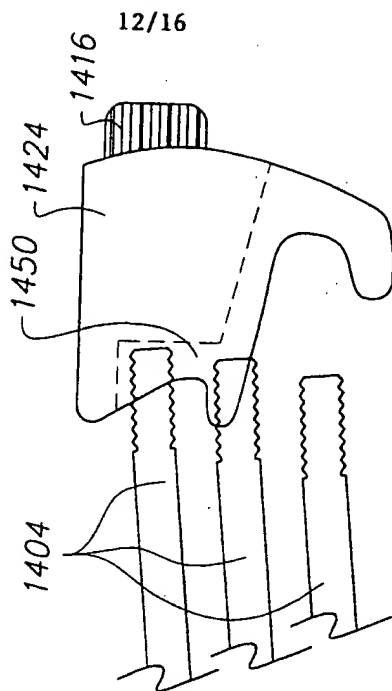
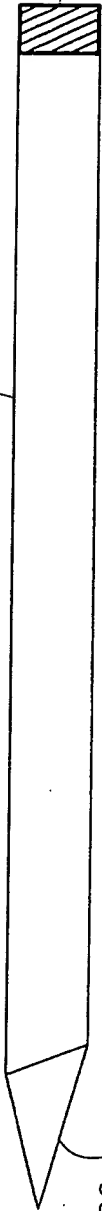


FIG. 14F

FIG. 15A

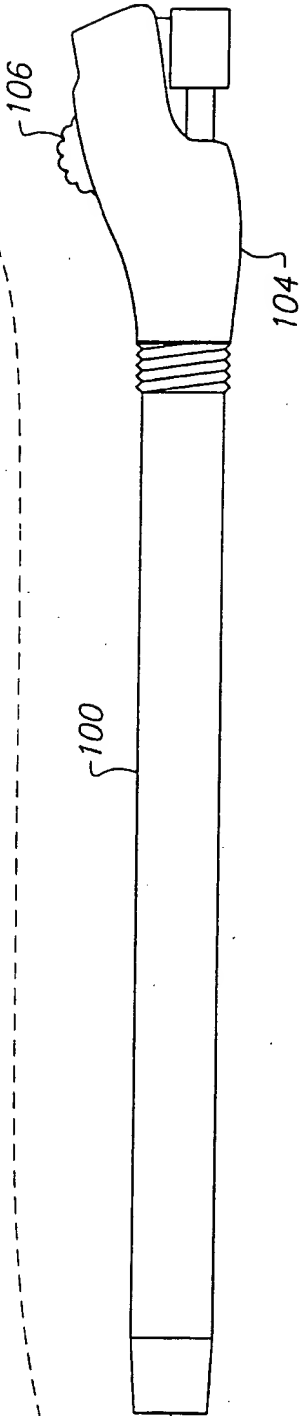
1500



1200

FIG. 15B

100



104

106

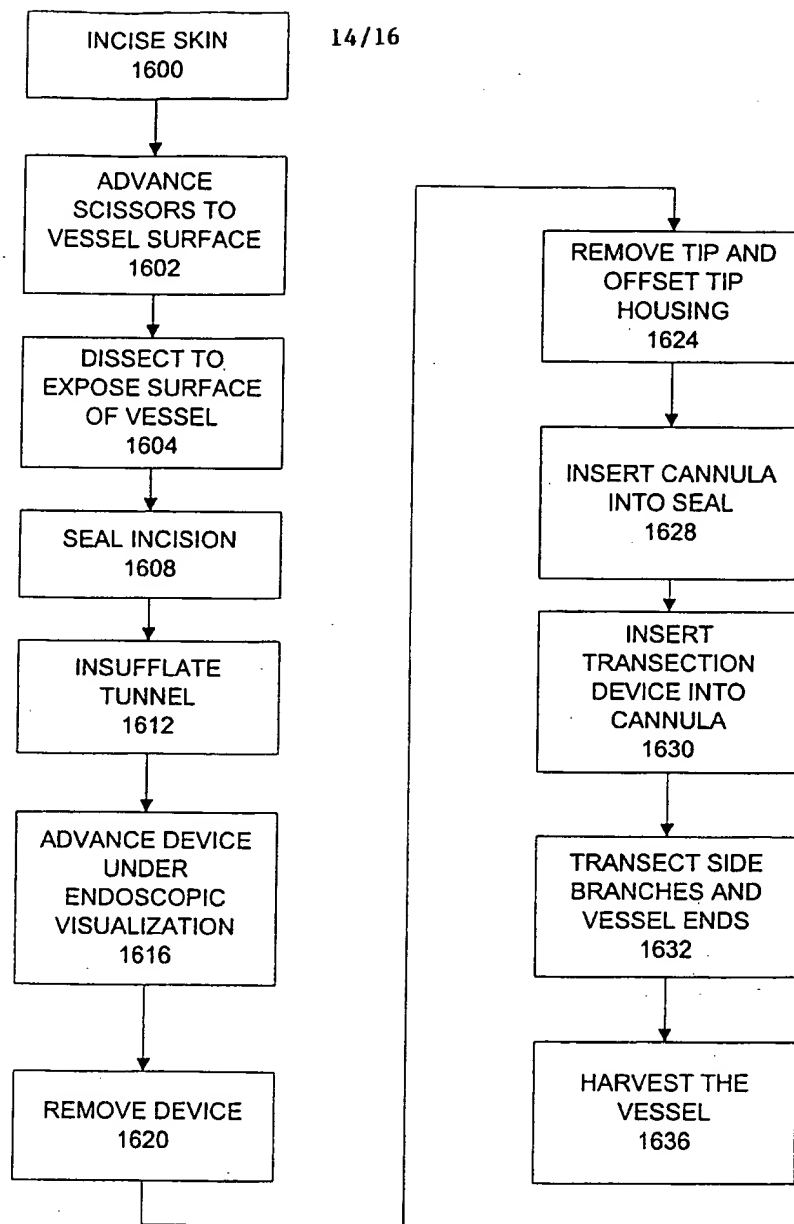
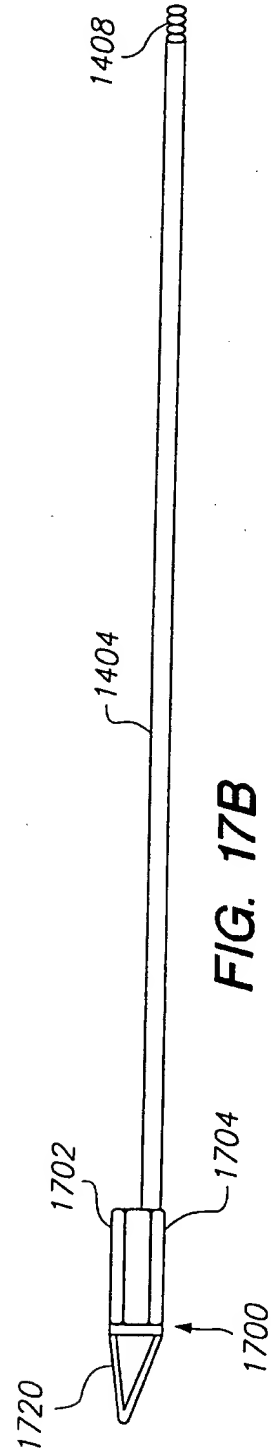
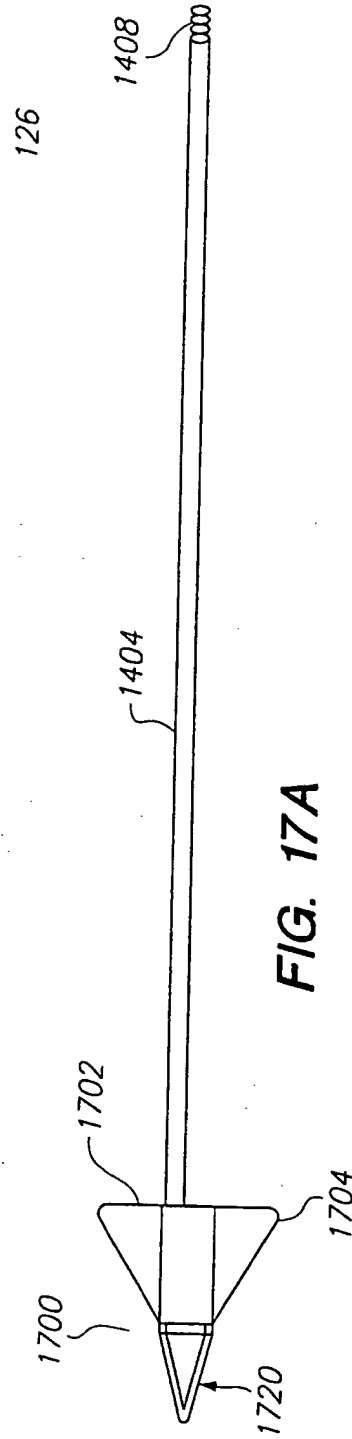
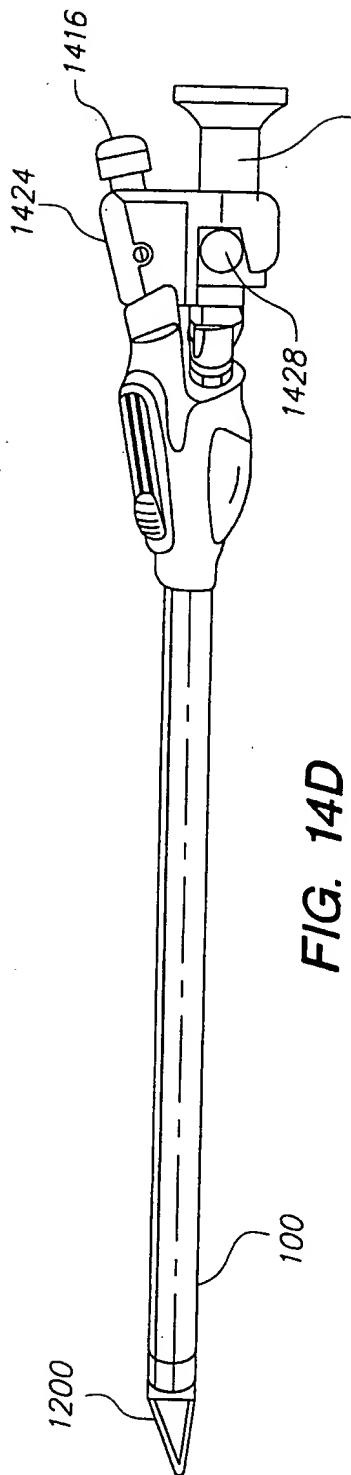


FIGURE 16



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**Zweikammerstützlager mit hydraulischer Dämpfung, insbesondere Motorlager in Kraftfahrzeugen.**

Es wird ein Zweikammerstützlager mit hydraulischer Dämpfung, insbesondere ein Motorlager in Kraftfahrzeugen beschrieben, dessen mit Flüssigkeit gefüllte Arbeitskammer (1) und Ausgleichskammer (2) Wandungen (3,4) aus ringförmigen Gummimembranen mit einer in Anpassung an die Betriebsbelastungen regelbaren Beulcharakteristik aufweisen und über einen Düsenkanal (8) miteinander verbunden sind. Dabei sind in der Wandung der Arbeitskammer (1) Mittel zur Regelung der Beulcharakteristik (Beulsteifigkeit) vorgesehen, die nach einer bevorzugten Ausführungsform aus einer zusätzlichen Beulfeder (9) bestehen, welche in einem festen Bodenteil (7) eingespannt und von außen durch eine Schraube (13) in ihrem Beulverhalten regelbar ist.

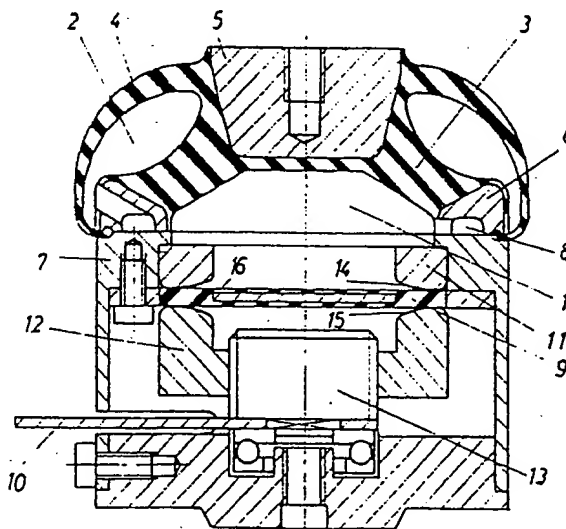


Fig. 1

## Zweikammerstützlager mit hydraulischer Dämpfung, insbesondere Motorlager in Kraftfahrzeugen

Die Erfindung betrifft ein Zweikammerstützlager mit hydraulischer Dämpfung, insbesondere ein Motorlager in Kraftfahrzeugen, mit Gattungsmerkmalen nach dem Patentanspruch 1.

Motorlager mit diesen Merkmalen sind aus der DE-OS 34 10 781 bekannt. Es weist einen Düsenkanal in einem starren Zwischenboden auf, der die obliegende Arbeitskammer von der darunter angeordneten Ausgleichskammer trennt. Die Dämpfungscharakteristik dieses Lagers ist dadurch einstellbar, daß der Düsenkanal durch gegeneinander offene Ausnehmungen in zwei gegeneinander um eine Hochachse verdrehbaren Scheiben gebildet ist, die beim Einbau des Lagers in eine auf individuelle Dämpfung ausgerichtete Stellung zueinander gebracht werden. Nach dem Lagereinbau ist eine Einstellung nicht mehr möglich. Das über den gesamten Frequenzbereich lineare Verhalten des Lagers ist dadurch jedoch einstellbar. Bekannt ist hieraus auch die Entkopplung von Schwingungen mit sehr kleinen Amplituden durch einen gummielastisch gehaltenen Wandungsteil, der gegen die äußere Atmosphäre ausweichen kann, wobei die Widerstandskraft sich jedoch überproportional aufbaut und die Wirksamkeit der Entkopplung auf ganz kleine Amplituden beschränkt.

Bekannt sind schließlich Düsenkanäle zwischen den beiden Kammern eines Motorlagers mit elektronisch permanent regelbarer Durchflußmenge zur Beeinflussung der Dämpfungscharakteristik des Motorlagers. Der erforderliche technische Aufwand übersteigt jedoch bei weitem die Kosten eines Lagers nach der zuerst erwähnten Druckschrift.

Der Erfindung liegt die Aufgabe zugrunde, bei Zweikammerstützlager der genannten Gattung eine großflächige Abkopplung beider Amplituden zu erreichen und diese Abkopplung permanent regeln zu können.

Diese Aufgabe löst die Erfindung durch die Ausbildungsmerkmale nach dem Kennzeichen des Patentanspruches 1.

Herausragend ist der Vorteil, daß eine solche Ausbildung die Regelung der Beulcharakteristik auch nach dem Einbau des Lagers ermöglicht, so daß durch ständige Verstellung eine laufende Anpassung der Dämpfungscharakteristik an wechselnde Betriebszustände durchgeführt werden kann. Dazu können gegebenenfalls Sensoren im Fahrzeug den Betriebszustand mittels Stellglieder auf das Regelorgan für die Beulcharakteristik im Lager übertragen. Auch eine Anpassung von Hand an ein gewünschtes Verhalten ist dadurch jederzeit möglich.

Bei einer bevorzugten Ausführungsform erstreckt sich die Ausgleichskammer ringförmig um eine mittige Arbeitskammer, wobei die Mittel zur Regelung der Beulcharakteristik in einem dadurch von außen frei zugänglichen Bodenteil der Arbeitskammerwandung angeordnet sind. Bei einer solchen Ausbildung ist der Düsenkanal in einem ringförmigen Tragelement angeordnet, welches mit der ringförmigen Gummimembran der Wandung der Arbeitskammer und mit einem flachen Bodenteil fest verbunden ist. Dadurch ist das Bodenteil von außen frei zugänglich und somit für die Aufnahme regelbarer Mittel zur Steuerung der Beulcharakteristik der Wandungen der Arbeitskammer geeignet.

Erfindungsgemäß ist in diesem starren Bodenteil der Arbeitskammer eine weitere Beulfeder aus einer Membran angeordnet, die mit ihrem Rand eingespannt und in ihrem Beulverhalten regelbar ist. Zweckmäßig ist eine Beulfeder aus einer runden Membranscheibe, deren Einspannung am Rande im Durchmesser über ein Stellglied von außen veränderbar ist. Durch Veränderung des Einspanndurchmessers kann somit die Beulcharakteristik der zusätzlichen Beulfeder bestimmt werden. In weiterer Ausgestaltung der Erfindung ist diese zusätzliche Beulfeder in der Form einer Membranscheibe am Rand zwischen zwei axial im Abstand zueinander einstellbaren Druckringen eingespannt, wobei die Spannflächen der beiden Druckringe mit der Mittelebene der Membranscheibe einen mit dem Scheitel nach außen weisenden Winkel einschließen.

Vorteilhaft sind Spannflächen der Druckringe, die im Querschnitt gekrümmt sind, wobei der Abstand von der Mittelebene der Membranscheibe von außen nach innen zunimmt. Der eine Druckring ist dabei in dem Gehäuse fest verankert, während der andere Druckring mittels einer Schraube von außen gegen den festen Druckring verstellbar ist. Durch die Oberflächenkontur der die Membranscheibe berührenden Spannflächen kann somit der Einspanndurchmesser variiert werden, um das Beulverhalten der Membranscheibe zu beeinflussen. Für die Betätigung ist nach einem weiteren Gedanken eine Schraube mit einem seitlich herausragenden Betätigungsorgan vorgesehen, an welches entweder selbsttätig wirksame Regelglieder oder ein Gestänge zur Beeinflussung von Hand angelenkt sein können. Ein weiteres besonderes Erfindungsmerkmal ist in der Anordnung einer Versteifungseinlage in der Membranscheibe zu sehen, wodurch die Membranscheibe an besondere Be-

triebsverhältnisse vorgegeben eingestellt werden kann. Diese Versteifungseinlage kann starr oder mit einer eigenen Elastizitätscharakteristik ausgestattet sein.

Auf der Zeichnung ist ein Ausführungsbeispiel der Erfindung dargestellt. Es zeigen:

Figur 1 einen vertikalen Schnitt durch ein Zweikammerstützlager,

Figur 2 ein dimensionsloses Regelschaubild der Schwingungsphase über der Frequenz und

Figur 3 ein dimensionsloses Regelschaubild der Beulsteifigkeit über der Frequenz.

Das Ausführungsbeispiel in der Figur 1 zeigt ein Zweikammerstützlager mit hydraulischer Dämpfung, insbesondere ein Motorlager in Kraftfahrzeugen, dessen mit Flüssigkeit gefüllte Arbeitskammer 1 und Ausgleichskammer 2 Wandungen 3 und 4 aus ringförmigen Gummimembranen aufweisen. Dabei erstreckt sich die Ausgleichskammer 2 ringförmig um eine mittige Arbeitskammer 1, so daß die die Wandungen 3 und 4 bildenden Gummimembranen einstückig ausgebildet sein können. Dieser Gummikörper ist mit dem oberen zentral angeordneten Tragelement 5 festhaftend verbunden, welches am Motor oder an einem anderen abzustützenden Teil befestigbar ist. Die die Wandung 3 der Arbeitskammer 1 bildende Gummimembran ist mit ihrem freien Ende festhaftend mit einem zweiten Tragkörper 6 verbunden, welcher mit einem ringförmigen Bodenteil 7 der Arbeitskammer verschraubbar ist und in der Teilungsebene eine ringförmige Ausnehmung 8 aufweist, die den Düsenkanal zwischen den beiden Kammern 1 und 2 bildet. Die die Wandung 4 bildende Gummimembran der Ausgleichskammer ist mit ihrem freien Rand zwischen dem Tragkörper 6 und dem Bodenteil 7 eingeklemmt.

In diesem Bodenteil 7 ist eine weitere Beulfeder 9 aus einer runden Membranscheibe angeordnet, deren Einspannung am Rande im Durchmesser über ein Stellglied 10 von außen veränderbar ist. Diese Beulfeder 9 ist am Rande zwischen zwei axial im Abstand zueinander einstellbaren Druckringen 11 und 12 eingespannt. Der eine Druckring 11 ist fest im Bodenteil 7 angeordnet, während der andere Bodenteil 12 mittels einer Schraube 13 in Richtung seiner Hochachse gegen den Druckring 11 verstellbar ist. Die Spannflächen 14 und 15 der beiden Druckringe 11 und 12 schließen mit der Mittelebene der Beulfeder 9 einen mit dem Scheitel nach außen weisenden Winkel ein. Vorteilhaft ist eine gekrümmte Ausbildung dieser Spannflächen in der Weise, daß der zwischen den Spannflächen 14 und 15 verbleibende Abstand voneinander von außen nach innen größer wird, d.h. der Abstand der gekrümmten Spannflächen von der Mittelebene der Beulfeder 9 nimmt von außen nach innen zu. Durch Verdrehen der Schraube 13 mittels des Stellgliedes

10 kann der Druckring 12 gegen den festen Druckring 11 bewegt werden, um dadurch den Einspanndurchmesser der Beulfeder 9 zu verringern bzw. bei umgekehrter Bewegung des Druckringes 12 zu vergrößern. Die dadurch bewirkte Veränderung der Beulsteifigkeit der Membranwandungen der Arbeitskammer 1 ist in den Schaubildern entsprechend Figur 2 und Figur 3 dargestellt. Bei annähernd gleicher Frequenz kann durch Verstellung des Druckringes 12 eine unterschiedliche Schwingungsphase der Beulfeder 9 eingestellt werden (Figur 2). Das Schaubild in der Figur 3 zeigt die Beulfedereinstellung in mehreren Stufen von weich bis hart. Das hier gezeigte Verhalten der Beulfeder 9 kann durch eine eingelagerte schwingende Masse 16 zusätzlich beeinflusst werden, wobei diese in das Material der Beulfeder eingebettete Masse 16 zu Beispiel aus einer im wesentlichen starren Versteifungseinlage gestaltet sein, aber auch aus einem elastischen Werkstoff bestehen kann, welcher ein vom Material der Beulfeder abweichendes spezifisches Gewicht und/oder eine davon abweichende Härte aufweist. Äquivalent wäre eine Beulfeder mit einem starren mittleren Teil und einer elastischen Randzone, die zwischen Druckringen 11 und 12 eingespannt ist, wobei die Spannflächen alternativ zu den gekrümmten Spannflächen der Druckringe nach Figur 1 auch eben gestaltet sein können.

## Ansprüche

1. Zweikammerstützlager mit hydraulischer Dämpfung, insbesondere Motorlager in Kraftfahrzeugen, dessen mit Flüssigkeit gefüllte Arbeitskammer und Ausgleichskammer Wandungen aus ringförmigen Gummimembranen mit einer in Anpassung an die Betriebsbelastung regelbaren Beulcharakteristik aufweisen und über einen Düsenkanal miteinander verbunden sind, dadurch gekennzeichnet, daß in der Wandung der Arbeitskammer (1) Mittel (9,10,13) zur Regelung der Beulcharakteristik (Beulsteifigkeit) vorgesehen sind.

2. Zweikammerstützlager nach Anspruch 1, dadurch gekennzeichnet, daß die Ausgleichskammer (2) sich ringförmig um eine mittige Arbeitskammer (1) erstreckt und daß die Mittel zur Regelung der Beulcharakteristik in einem dadurch von außen zugänglichen Bodenteil (7) der Arbeitskammerwandung angeordnet sind.

3. Zweikammerstützlager nach den Ansprüchen 1 und 2, dadurch gekennzeichnet, daß die Mittel (9,10,13) zur Regelung der Beulcharakteristik der Arbeitskammer (1) aus einer in dem Bodenteil (7) ihrer Wandung befestigten Membran besteht, die mit ihrem Rand eingespannt und in ihrem Beulverhalten regelbar ist.



4. Zweikammerstützlager nach den Ansprüchen 1 bis 3, gekennzeichnet durch eine Beulfeder (9) aus einer runden Membranscheibe, deren Einspannung am Rand im Durchmesser über ein Stellglied (10,13) von außen veränderbar ist.

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5. Zweikammerstützlager nach den Ansprüchen 1 bis 4, dadurch gekennzeichnet, daß die die Beulfeder (9) bildende Membranscheibe am Rand zwischen zwei axial im Abstand zueinander einstellbaren Druckringen (11,12) eingespannt ist, wobei die Spannflächen (14,15) der beiden Druckringe (11,12) mit der Mittelebene der Membranscheibe einen mit dem Scheitel nach außen weisenden Winkel einschließen.

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6. Zweikammerstützlager nach Anspruch 5, dadurch gekennzeichnet, daß die Spannflächen (14,15) der Druckringe (11,12) im Querschnitt gekrümmt sind, wobei der Abstand von der Mittelebene der Membranscheibe (9) von außen nach innen zunimmt.

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7. Zweikammerstützlager nach den vorhergehenden Ansprüchen 1 bis 6, dadurch gekennzeichnet, daß der eine Druckring (11) im Gehäuse fest und der andere Druckring (12) mittels einer Schraube (13) von außen gegen den festen Druckring (11) verstellbar ist.

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8. Zweikammerstützlager nach Anspruch 7, dadurch gekennzeichnet, daß die Schraube (13) mit einem seitlich herausragenden Betätigungsorgan (10) verbunden ist.

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9. Zweikammerstützlager nach den vorhergehenden Ansprüchen, dadurch gekennzeichnet, daß die die Beulfeder (9) bildende Membranscheibe eine in deren Werkstoff eingelagerte schwingende Masse (16) aufweist.

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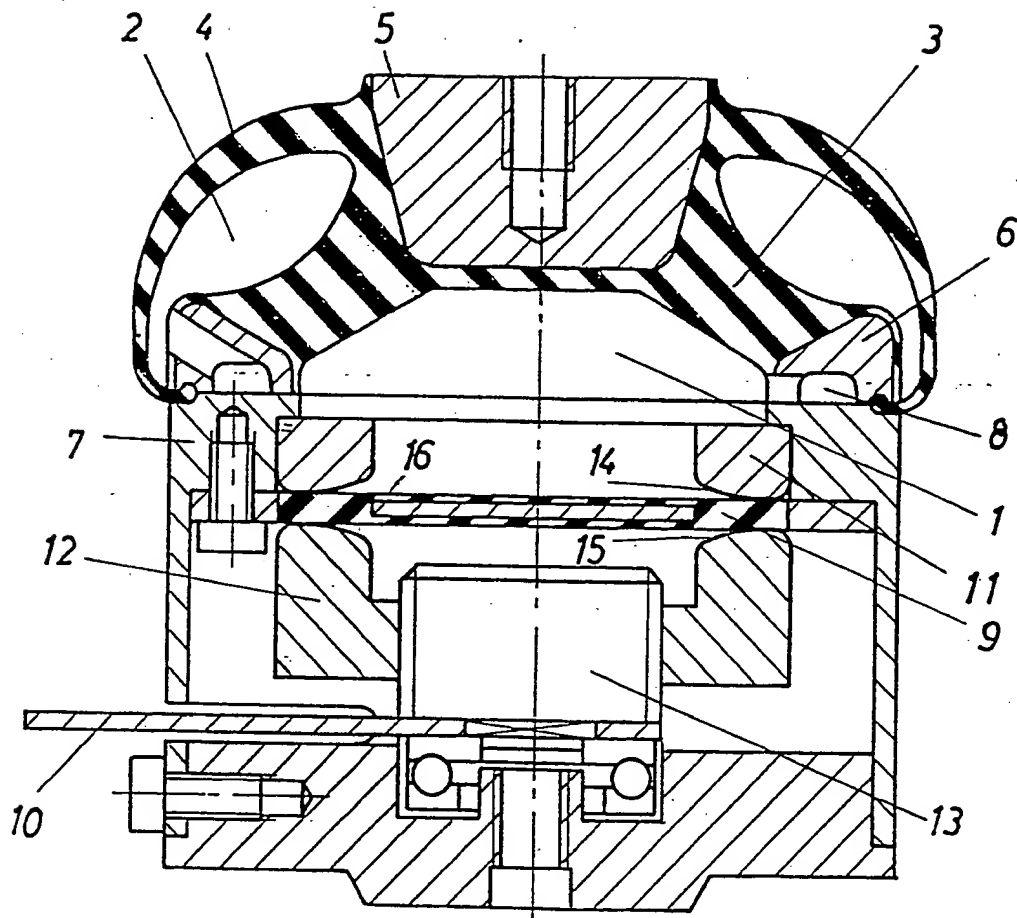
10. Zweikammerstützlager nach Anspruch 9, dadurch gekennzeichnet, daß die eingelagerte Masse (16) als eine starre Versteifung gestaltet ist.

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*Fig. 1*

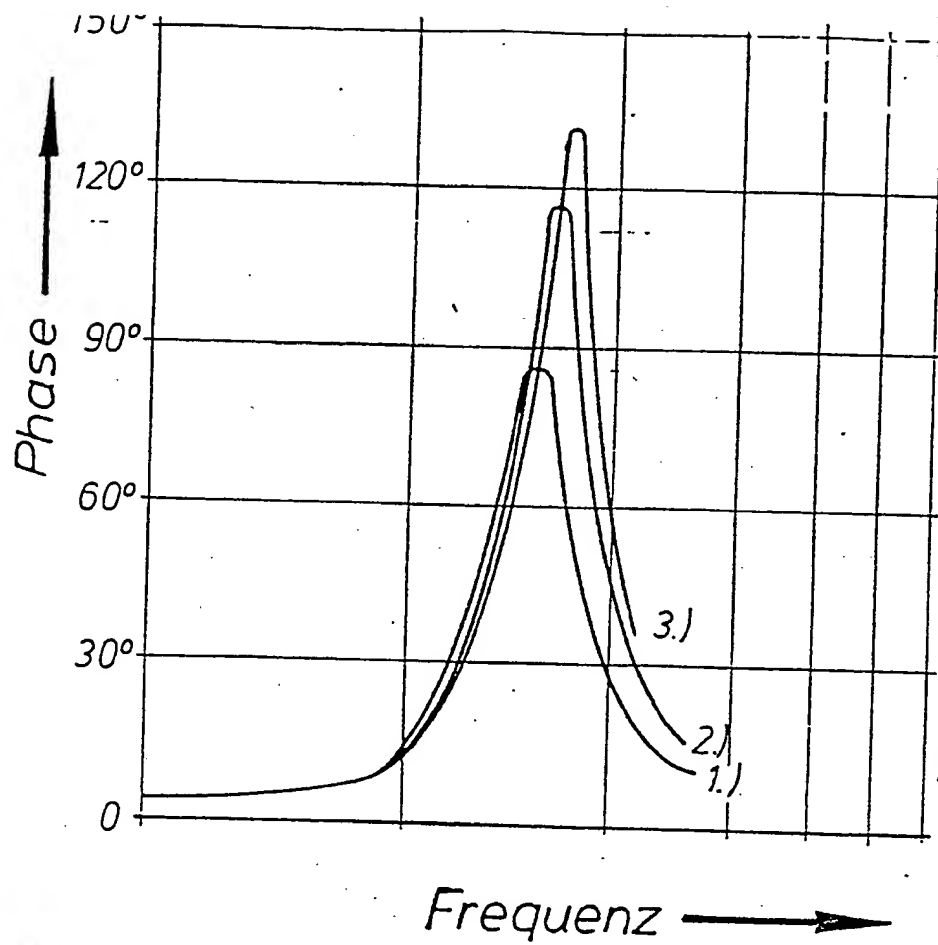
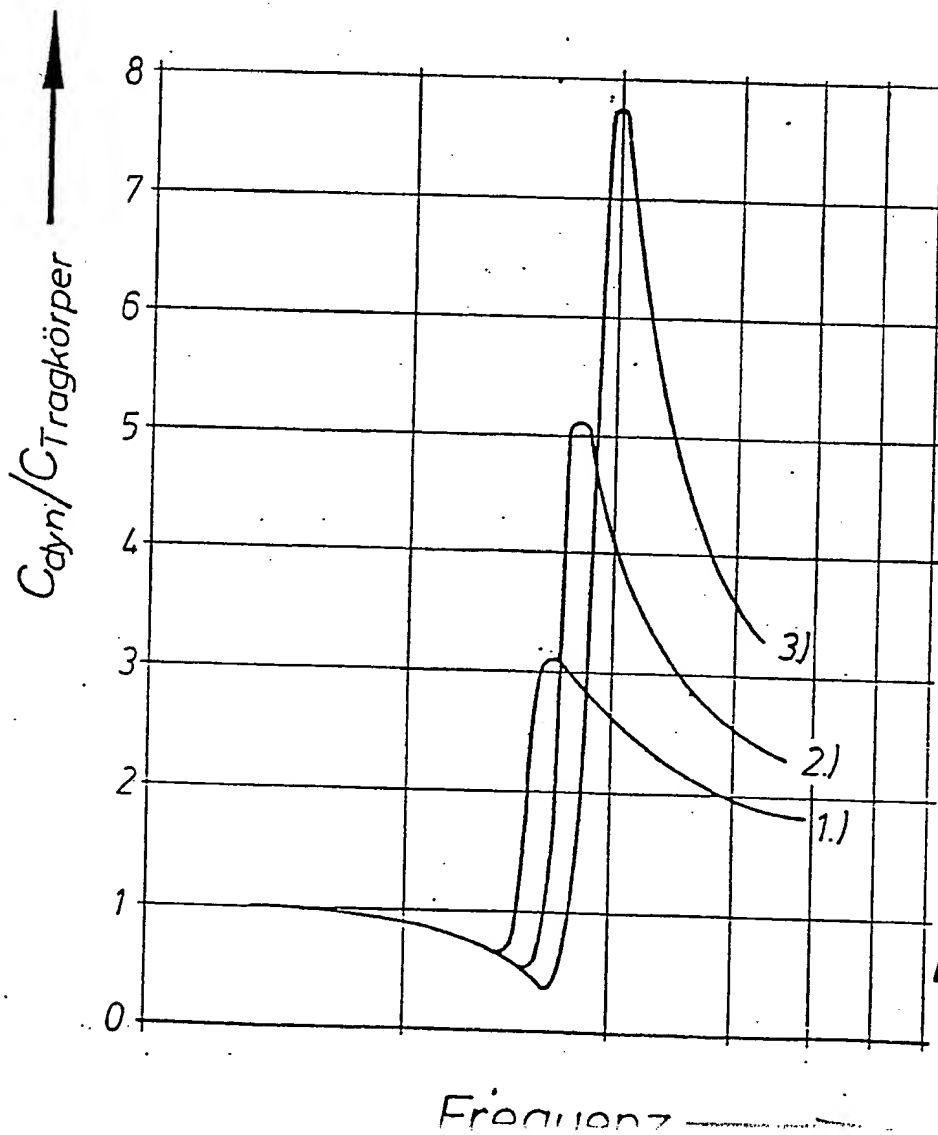


Fig. 2



Beulfeder-  
einstellung  
1.) weich  
2.) mittel  
3.) hart

Fig. 3